

Design Considerations for HIFU Transducers

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Introduction

Intent of this workshop is to outline some design considerations and guidelines for various types of transducers intended to be used for HIFU applications:

Medical: Ablation, drug delivery, etc

Industrial: droplet jets, descaling, etc

Consumer: drug delivery, atomization, etc

“ Invention is 10% inspiration and 90% perspiration” Thomas Edison

Bio

- **1982: BSE - Purdue University**
- **1982 – 1999: Etalon, Inc**
- **1999 – 2007: Piezotech, LLC**
- **2007 to present: Better UltraSonic Technologies**
- **26 years of piezo and ultrasound transducer design, manufacture and marketing**
- **17 years of medical HIFU**

Outline

- **Define Your Application**
- **Select best transducer configuration**
- **Determine Frequency and Sound Field**
- **Determine Power Requirements**
- **Select Piezo Material**
- **Determine Best Matching Layers**
- **Select Adequate Interconnects**
- **Tune Electrical Impedance**

Outline

- **Consider Thermal Management**
- **Model, Model, Model**
- **Consider MRI Compatibility**
- **Test and Characterize Performance, Life and Safety**

- **Consider Other Uses**
- **References**
- **Questions / Discussion**

Define Your Application

- **Assuming Medical**
- **Extracorporeal – Laparoscopic – Endocavity**
 - Low F, long FL; High F, short FL; Mid, FL
- **Durable – Disposable**
- **Biocompatibility of contact materials needs to be Class VI**
- **Imaging Modality**
 - Integral to HIFU F
 - Integrated with HIFU
 - Other Modality: MRI, PET, CT, etc
 - Compatibility issues?

Define Your Application

- **Identify Target Tissue(s) and Properties**
- **Identify Target Depth**
- **Identify any Intervening Materials and Properties**
- **Determine Treatment Volume Estimate**
- **Minimum Site Intensity (I_s)**

Define Your Application

- **Determine Treatment Time**
 - (ref's: 10,11,12,51,52)
 - +70 C = 1 S, +56 C = 3 S, +43 C = 7200 S
 - After L. Crum, Therapeutic Workshop, 2007 US Symposium
- **Consider Best Packaging**

Select Best Transducer Configuration

- **Single Element**

- Flat piezo element with Lens: low cost, less eff.
- Cylindrical segment: medium cost, line focus
- Spherical section: high cost, point focus, requires controlled scanning

- **Multi-Element**

- Annular Array: medium to high cost, point focus, allows movement of focus along beam axis
- Linear Array: expensive, can be concave, convex, phased, allows focusing along beam axis and transducer length, requires controlled scanning on transducer width for 3D

Select Best Transducer Configuration

- **2D Array: very expensive, phasing allows focusing in 3D**
- **CAUTION: Arrays create grating lobes – points of focus other than those intended- that can create hot spots/ lesions outside of the intended treatment area**
- **References: 13 – 22, 37**

Determine Frequency and Sound Field

- Application is defined – how (ex, lap, endo), depth, intervening matl's, vol., I_s , Thermal
- Can calculate Frequency, F; Aperture, D; Focal Depth, FL; and Power, P_o
- Frequency
 - Mainly dependent on depth to target due to intervening tissue attenuation
 - Typical is $\alpha = .5$ to 1.5 dB/cm-MHz, 1 dB/cm-MHz is used

Determine Frequency and Sound Field

Example

Let $z = 6 \text{ cm}$, $F = 1 \text{ MHz}$

Loss to target = $-1 \text{ dB/cm-MHz} * 1 \text{ MHz} * 6 \text{ cm}$
= $-6 \text{ dB} = 10 \log (P/P_0)$

Based on assumptions and estimates made, the Site Intensity, I_s , needs to be estimated

Is typically between 1 kW/cm^2 and 10 kW/cm^2
For simplicity, let $I_s = 1 \text{ kW/cm}^2$

Determine Frequency and Sound Field

Need to set an Aperture, D , as well; may be affected by packaging or anatomy, etc

Typically, F number = $1 = D/FL$ but can be from about .7 to 2 effectively

Since $FL = 6\text{cm}$, then $D = 6\text{ cm}$ as well

Assume element geometry is the concave section of a sphere

From I_s , calculate P_o

$$I = P/\text{area} \quad \text{where } \text{ba} = \text{area}$$

Determine Frequency and Sound Field

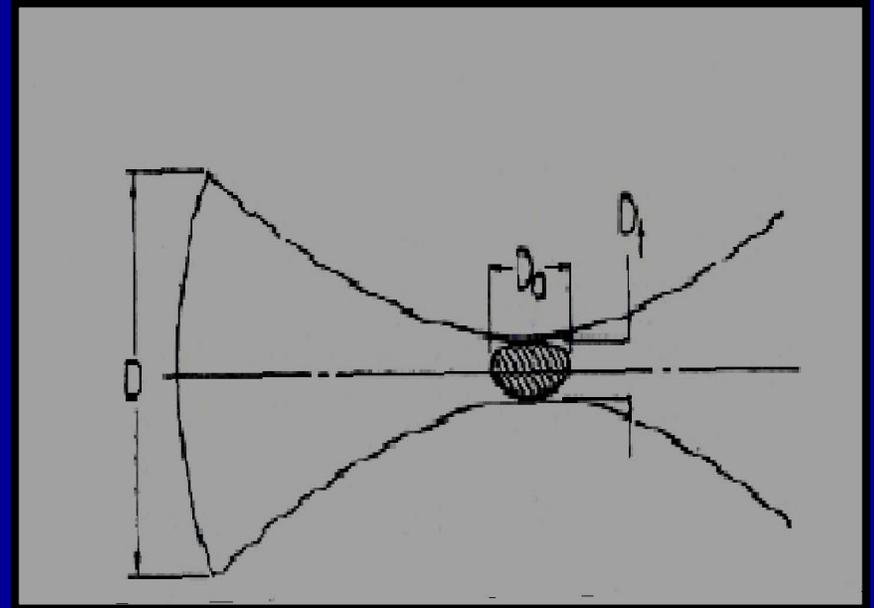
Calculate Focal beam Dia.,
Dt, Beam Area, ba, and
Focal Zone Length, FZL
(Da)

$$Dt = FL * c / (F * D), \text{ cm}$$

$$ba = \pi * d^2 / 4, \text{ cm}^2$$

$$Da = FZL \sim 10 d, \text{ cm}$$

$$\text{Vol} = ba * FZL, \text{ cm}^3$$



Determine Frequency and Sound Field

$$Dt = 6 * .15 / (1 * 6) = .15 \text{ cm}$$

$$ba = \pi * .15^2 / 4 = .018 \text{ cm}^2$$

$$Da = 10 * .15 = 1.5 \text{ cm}$$

This is an iterative process based on requirements of the application

Determine Power Requirements

Calculate Site Power, P_s , from I_s and ba

$$P_s = I * ba = 1000 * .018 = 18 \text{ W}$$

Calculate Power, P_o , from loss and P_s

$$\text{Loss} = -6 \text{ dB} = 10 \log (P_s/P_o)$$

$$P_o = P_s/10^{-.6} = 18 / .25 = 72 \text{ W}$$

Determine Power Requirements

Calculate Surface Intensity, I_a , on piezoelement

$$\text{surface area, } sa = \pi * D^2 / 4 = 29 \text{ cm}^2$$

$$I_a = P_o / sa = 72 / 29 = 2.55 \text{ W / cm}^2$$

this is well within limits of piezo materials

$$P_{\text{max}} = sa * I_s = 29 * 10 = 290 \text{ W}$$

The power and intensity limits need to be balanced against the possibility of damaging tissue between the transducer and target site.

Select Piezo Material

Limit to “high drive” types

Assume 50 ohm source and desired load

Calculate capacitance

$$C = 1 / \omega * Z$$

Where C is Farads, Z is impedance, $\omega = 2 * \pi * F$

$$C = 3200 \text{ pF}$$

Select Piezo Material

Calculate dielectric constant, K

$$K = C * t / (sa * \epsilon_0)$$

where t = thickness = .21 cm;
and $\epsilon_0 = 8.85 \times 10^{-14}$ F / cm

$$K = 260$$

Select Piezo Material

Type	PZT5	PbT	PZT 2a	PZT 2b	PZT8	PZT4	PZT 4D	PZ52 K320	PZ56 K340
Prop									
K3 ^T	1700	215	350	550	1000	1300	1450	1500	2900
K3 ^S	830	160	225	310	600	665	710	865	1500
K33	.70	.51	.63	.65	.62	.70	.71	.60	.65
Kt	.50	.51	.50	.52	.44	.45	.50	.50	.50
Qmr	75	0	>900	>750	1000	500	1000	2000	1600
Qmt	50	300	220	200	200	100	400	400	400

Select Piezo Material

	PZT 5A	PbT	PZT 2a	PZT 2b	PZT8	PZT4	PZT 4D	PZ52 K320	PZ56 K340
loss	.020	.015	.004	.004	.004	.008	.004	.002	.004
V/cm	450	10 k	8 k	8 k	10 k	3.9 k	>5 k	>10k	5 k
V/cm 100C	400	8 k	7 k	7 k	8 k	3.3 k	3.5k	10 k	4 k
W / cm ²	<1 >1	>25 >50	>10 >25	>10 >25	>20 >40	> 5 > 10	>10 >25	>25 >50	>10 >20
T _c ,C	350	350	350	330	300	325	300	320	200
d33	350	70	150	180	225	285	350	320	400
Z,MR	35	35	35	35	35	35	35	35	35
Vend	lots	E F P T M	F M P T	F M P T	lots	lots	lots	FP PT	FP PT

Select Piezo Material

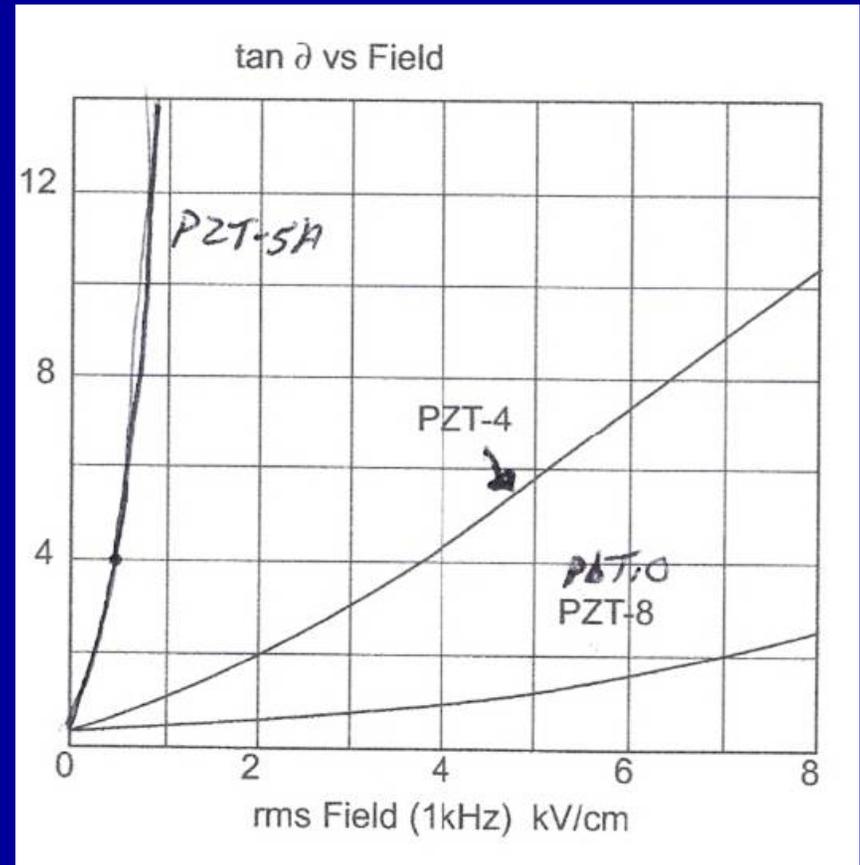
Calculate Power and
Voltage Limits

$$P_o = 2 * \pi * F * E^2 * k^2 * \epsilon_{33}^T * Q_m,$$

W/cm³

where E is V/cm,
 ϵ is F/cm

$$P_d = 2 * \pi * F * E^2 * \epsilon * l_f$$



(ref. 2)

Select Piezo Material

Need to balance Surface Intensity with applied Voltage using

$$P_o = V^2/R$$

where V = drive volts, rms

$$V = (P_o * R)^{1/2} = (72 * 50)^{1/2} = 60 \text{ Vrms}$$

$$V_{\text{max}} = t * E = .21 * 8000 = 1680 \text{ Vrms}$$

$$P_{\text{max}} = V_{\text{max}}^2/R = 56 \text{ kW}$$

$$V_{\text{max real}} = (290 * 50)^{1/2} = 120 \text{ Vrms}$$

Select Piezo Material

Composites (36)

Can be made from any
PZT, no gain for PbT

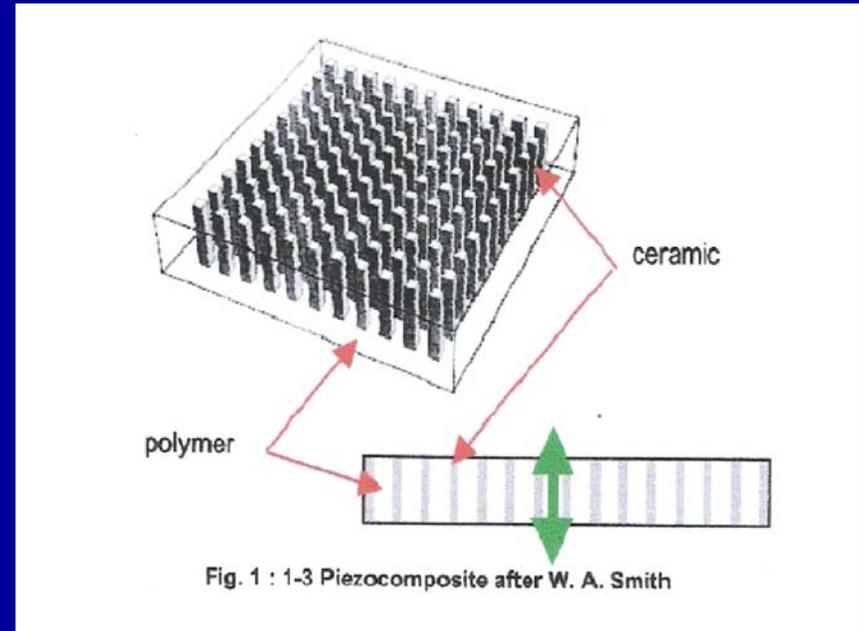
Pros: increase k , vary
volume % ceramic \rightarrow

K , Z_a , Z_e

minimal lateral modes,
minimal side lobes

Base for 2D array

30 W/cm² reported



Select Piezo Material

Cons

More expensive

Less solid ceramic → less real power

~ 1/3 thinner for same F → less Voltage

Have to manage heat effectively

Select Piezo Material

Single Crystals

Large $k = .7$ to $.9+$

Low loss, $< 1\%$ typically

But

High $K \rightarrow$ low Z_e , ok for array elements

Low T_c w/ phase change near 25 C

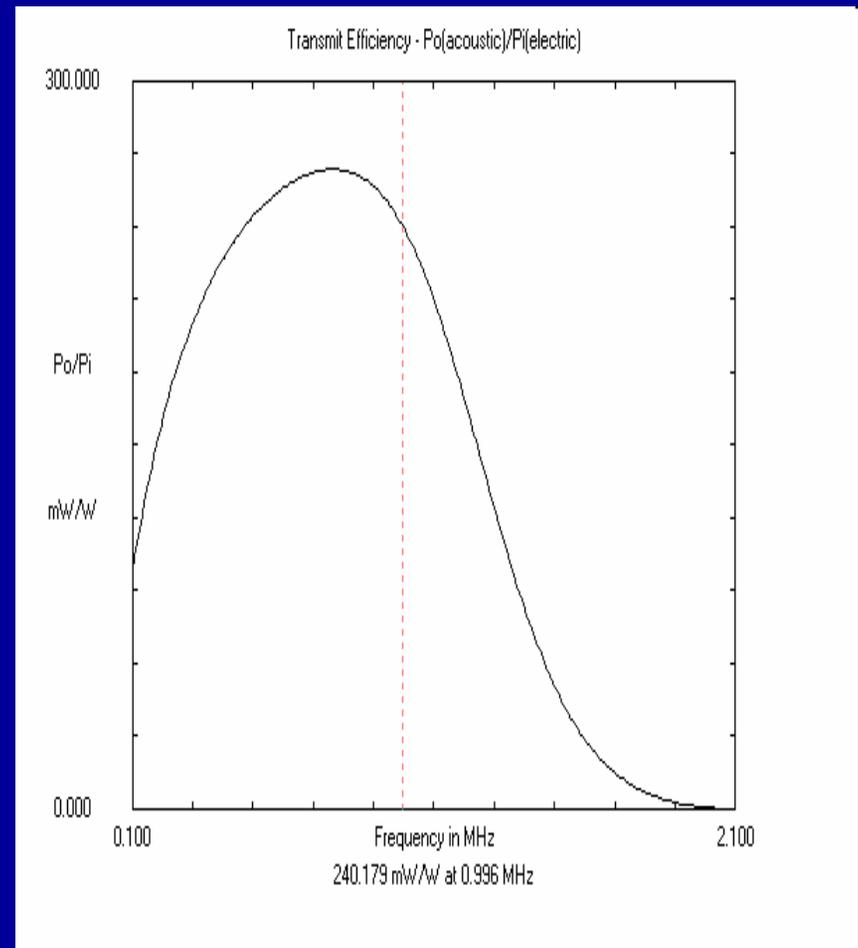
can they be focused?

very expensive: $\$1/\text{mm}^3 = \$1000/\text{cm}^3$

Determine Best Matching Layer(s) (3, 17)

1. None

- a. Ok if therapy only
- b. Still needs coating to protect electrode, leads, seal, etc
- c. Can get $> 50\%$ eff. If properly designed
- d. Very narrow BW
- e. Use PLL to stay on F_0
- f. Ex - CV



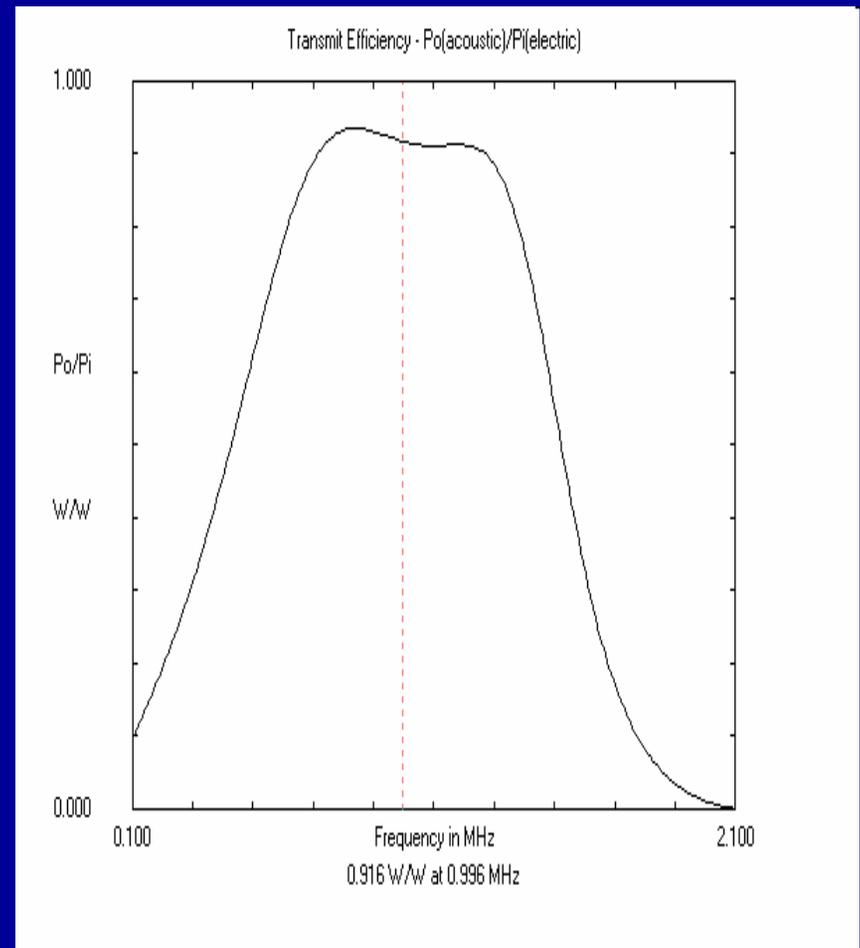
Determine Best Matching Layer(s)

2. Single $\lambda/4$

2 Main Equations

a. Geometric Mean

$$Z_{ml} = (Z_l * Z_x)^{1/2} \\ = 7.2 \text{ MR}$$



Determine Best Matching Layer(s)

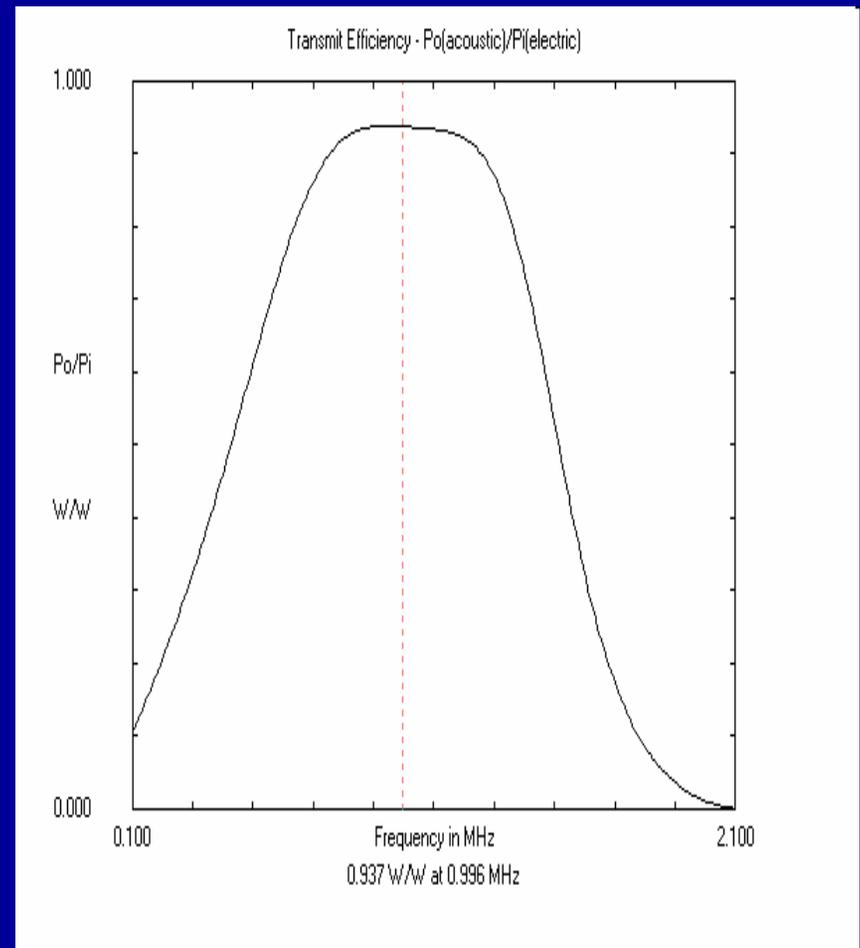
b. After DeSilet, et al

$$\begin{aligned} Z_{ml} &= Z_l^{2/3} * Z_x^{1/3} \\ &= 4.3 \text{ MR} \end{aligned}$$

used KLM, sets
 $Q_m = Q_e$ to max.

BW, min. PL

Not always best for max
 P_o



Determine Best Matching Layer(s)

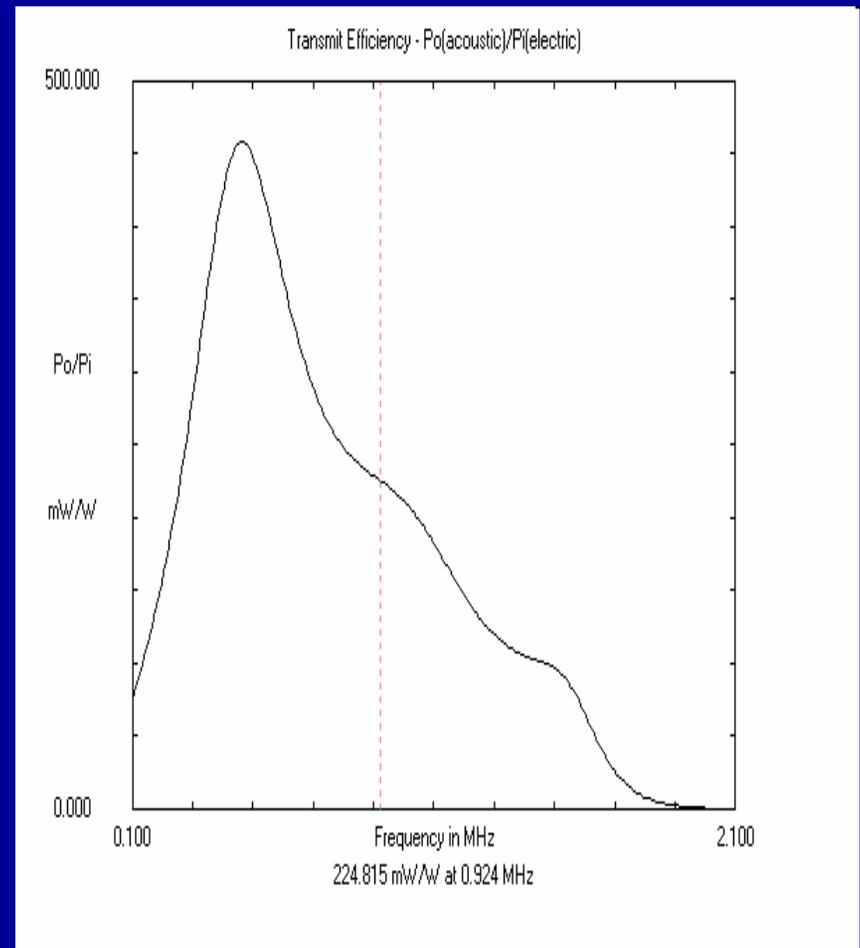
3. Single $\lambda/2$

same eq's.

a. Geometric Mean

$Z_{ml} = 7.2 \text{ MR}$

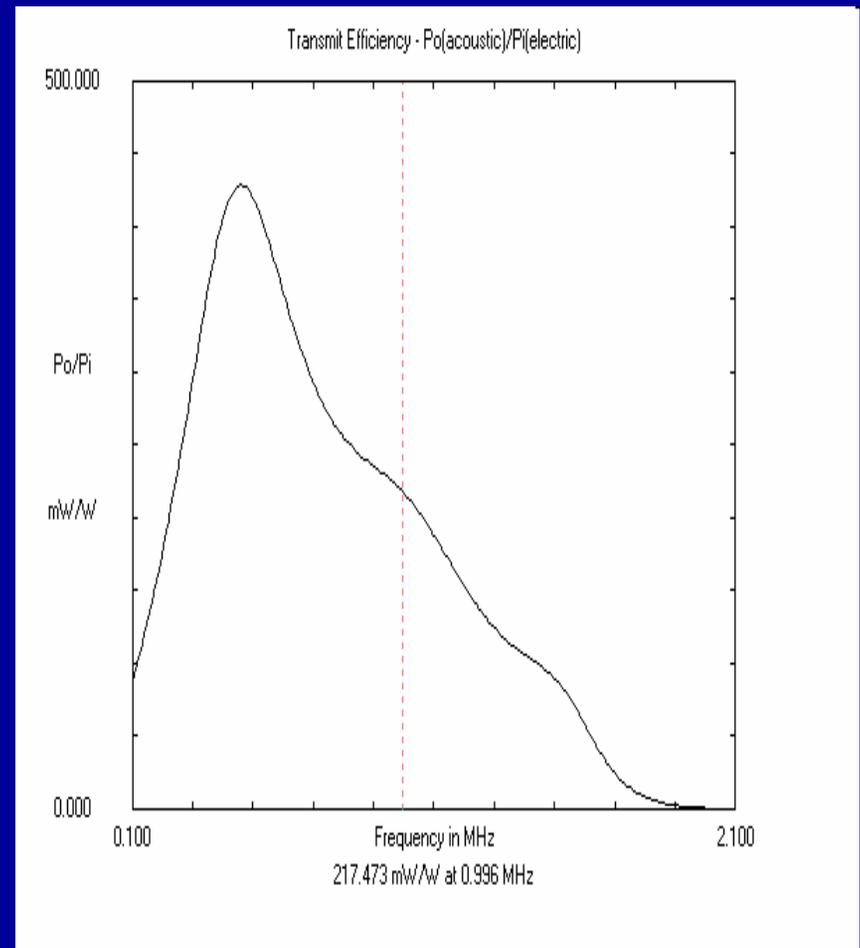
narrowband



Determine Best Matching Layer(s)

b. DeSilet

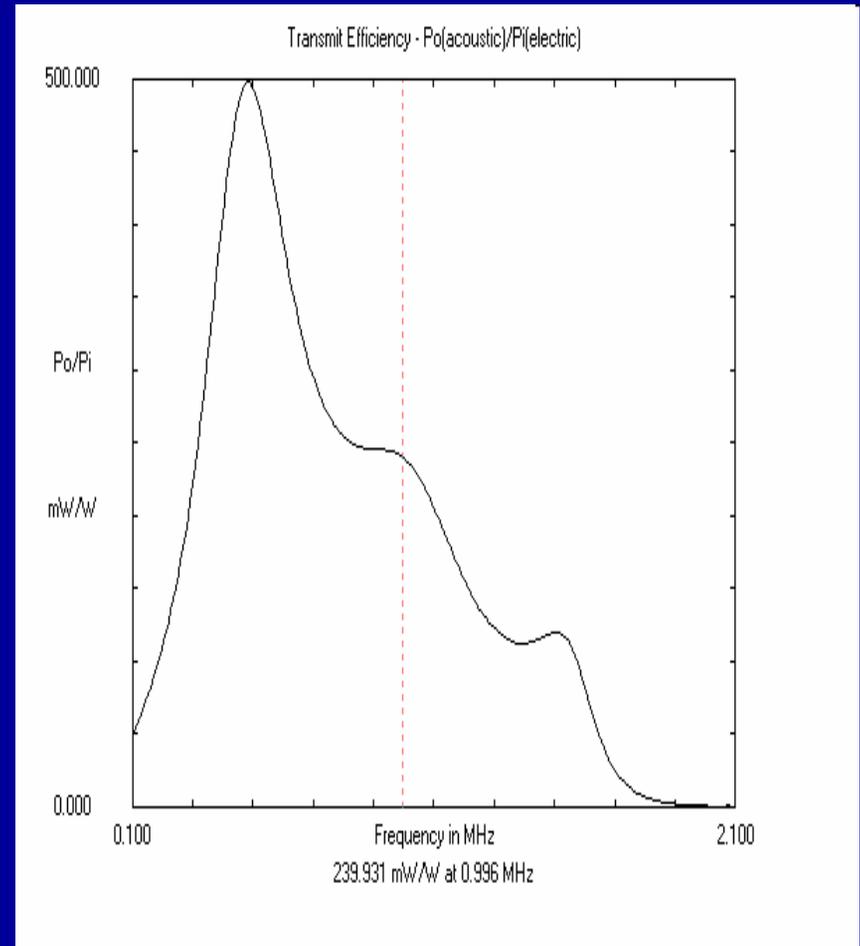
$Z_{ml} = 4.3 \text{ MR}$



Determine Best Matching Layer(s)

c. Example from
physiotherapy

Z_{ml} = 17.1 MR
Aluminum



Determine Best Matching Layer(s)

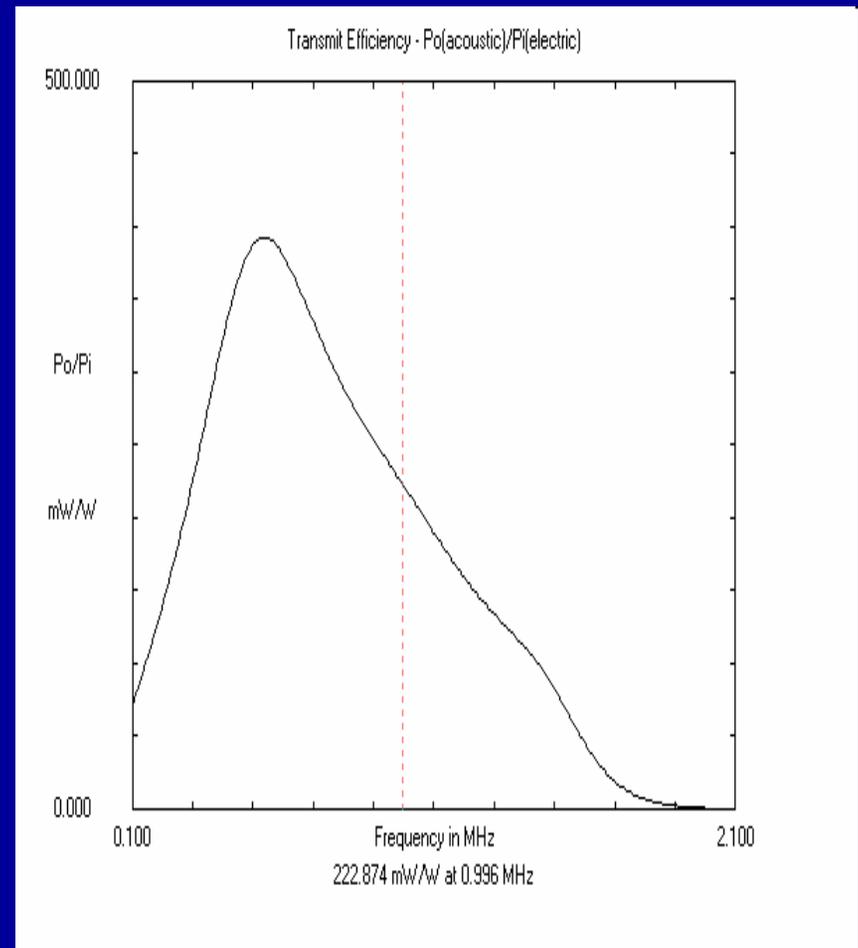
4. Double $\lambda/4$

3 Main Derivations
Max. BW

a. Geometric Mean

$$\begin{aligned} Z_{m1} &= Z_x^{2/3} * Z_l^{1/3} \\ &= 12 \text{ MR} \end{aligned}$$

$$\begin{aligned} Z_{m2} &= Z_x^{1/3} * Z_l^{2/3} \\ &= 4.2 \text{ MR} \end{aligned}$$



Determine Best Matching Layer(s)

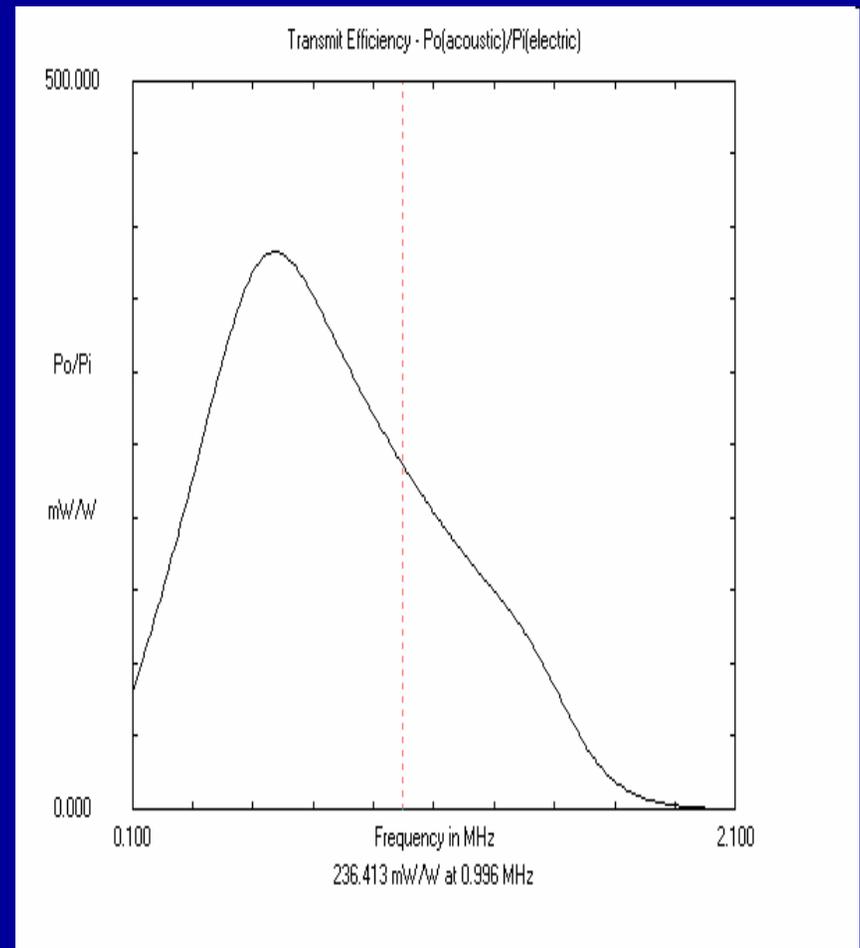
b. DeSilet

$$Z_{m1} = Z_x^{4/7} * Z_l^{3/7}$$

$$= 9 \text{ MR}$$

$$Z_{m2} = Z_x^{1/7} * Z_l^{6/7}$$

$$= 2.4 \text{ MR}$$

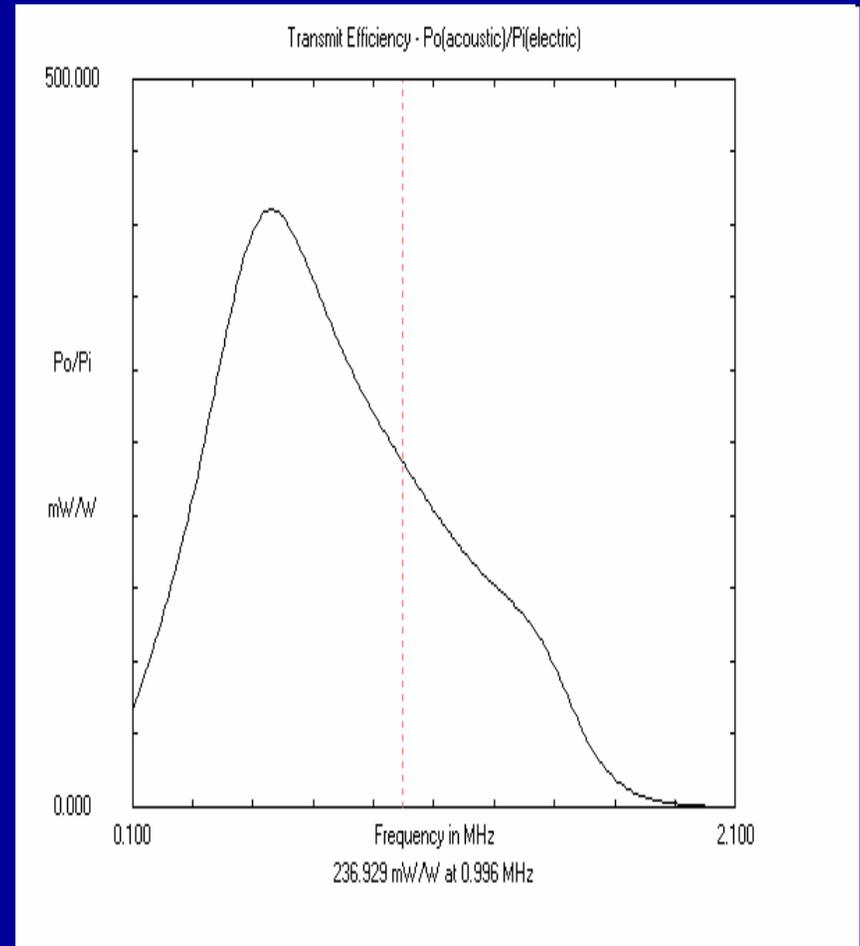


Determine Best Matching Layer(s)

c. After Goll

$$\begin{aligned} Z_{m1} &= Z_x^{3/4} * Z_l^{1/4} \\ &= 15.5 \text{ MR} \end{aligned}$$

$$\begin{aligned} Z_{m2} &= Z_x^{1/4} * Z_l^{3/4} \\ &= 3.5 \text{ MR} \end{aligned}$$



Determine Best Matching Layer(s)

5. Materials (4)

a. $Z = 1$ to 10 MR:

polymers, carbon, magnesium

fillers: AlO, AlN, SiC, W, Others

b. $Z = 10$ to 15 MR:

glass, glass ceramic, fused silica

c. $Z = 15$ to 20 MR:

x-cut quartz, aluminum, silicon, indium

Determine Best Matching Layer(s)

6. Precautions

High Power, i.e. Surface Intensity →

High surface deformation & heat

- a. electrode: high adhesion to piezo**
- b. ML: void free, high T_g , low α , some plasticity – Shore D 70 to 90**
- c. May require use of chemical primers**
- d. Mid to high thermal conductivity**

Select Adequate Interconnects

1. Electrodes on element

- a. Fired silver frit
- b. Sputtered or electroless copper, gold, nickel, platinum, palladium, indium, tin, etc
- c. Needs to be solderable, preferably nonmagnetic

2. Wires and Cables

- a. Foils: copper, tin, brass, nickel, silver
- b. Small gauge wires, solid or stranded, copper with tin, silver or gold plate, etc
- c. Cables: typ. Coax but can be twinax, triax, etc

Select Adequate Interconnects

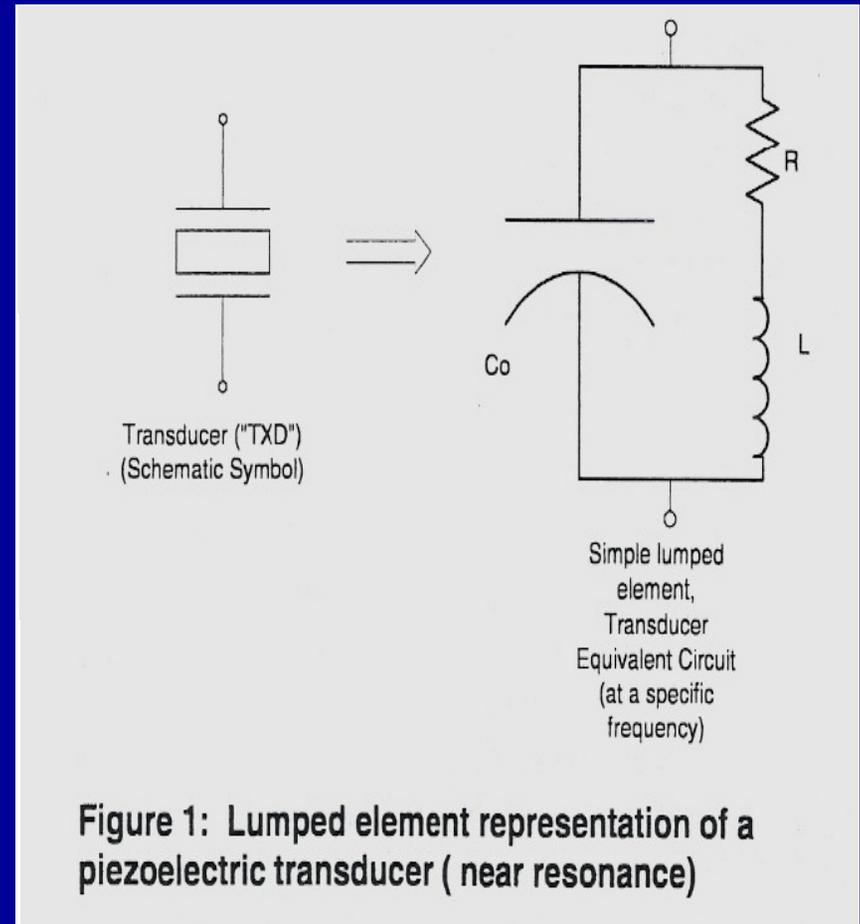
3. Solders

- a. **Pb/Sn, Sn/Ag, Pb/Sn/Ag, Sn/Ag/Cu, Au/In, etc.**
- b. **Conductive polymers**
- c. **Need to be somewhat pliable due to high mechanical stress**
- d. **Need to have high T_s / T_I due to high thermal stress**
- e. **Must be compatible with electrode and wire materials to prevent scavenging / leaching**

Tune Electrical Impedance

Transducer can be modeled as a simple Lumped-element Circuit

(ref's 5, 6, 7, 8, 9)



Tune Electrical Impedance

1. Parallel eq. Circuit

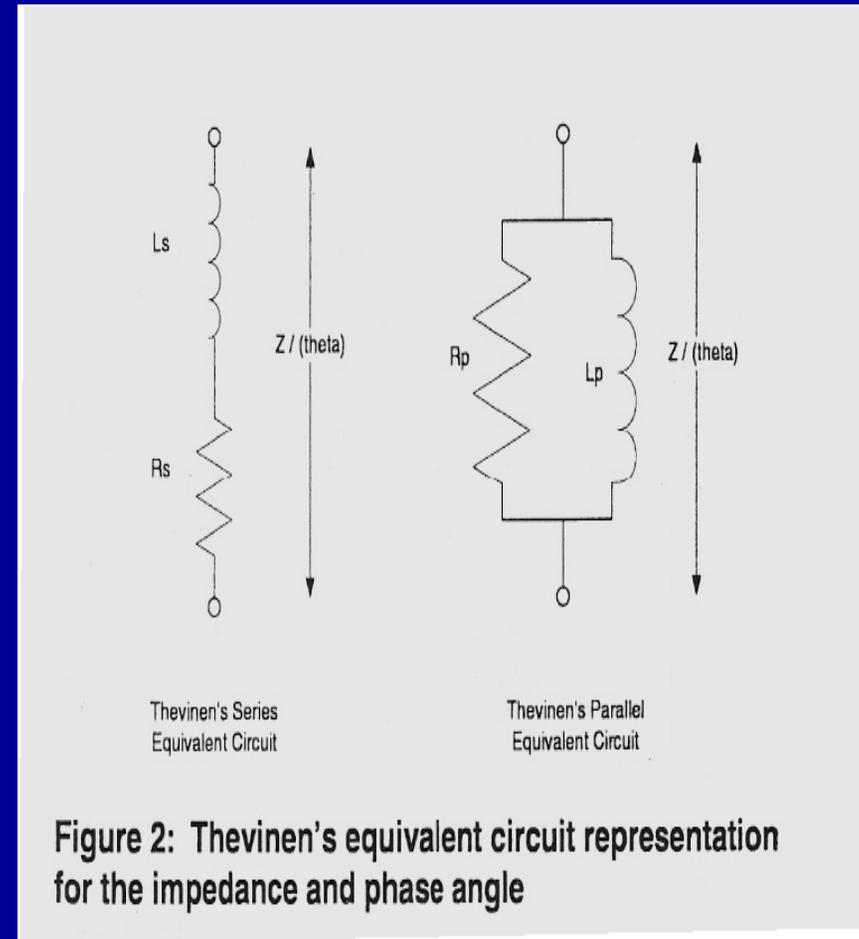
a. Parallel Inductor

$$R_p = Z / \cos \theta$$

$$X_p = Z / \sin \theta$$

$$L_p = X_p / \omega$$

**Requires high
saturation core &
large wire gauge**



Tune Electrical Impedance

b. Transformer

$$Z_{sec} / Z_{pr} = N^2$$

$$\text{set } Z_{sec} = \omega * X_p$$

$$\text{or } L_p = L_{sec} =$$

$$X_p / \omega$$

$$Z_{pr} = R_s$$

$$\text{and } N = t_s / t_p$$

$$= (\omega * L_p / Z_{pr})^{1/2}$$

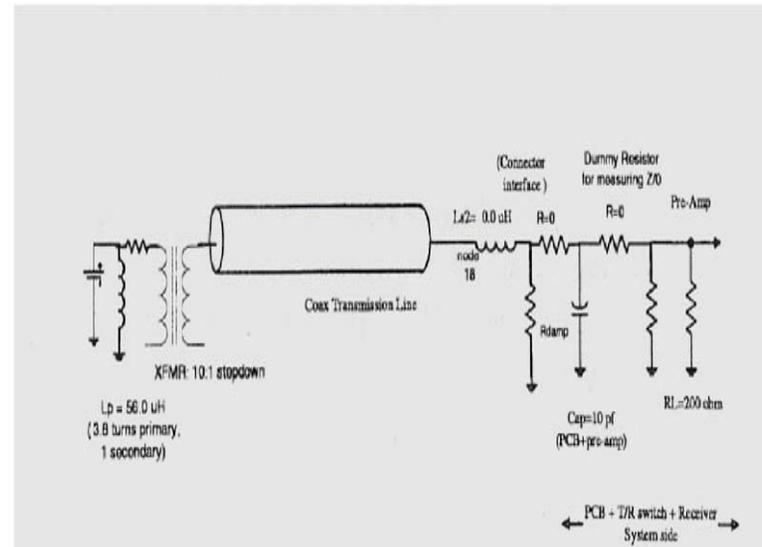


Figure 4: Broadband impedance matching (tuning) with "auto-transformer"

Tune Electrical Impedance

b. Transformer

can be toroid, C-core, E-core, balun, etc
be cautious with wire gauge and core material

typically high Q but can control with additional capacitance

$$Q = R_p / X_p$$

Tune Electrical Impedance

2. Series Eq. Circuit

$$R_{ser} = Z * \cos \theta$$

$$X_{ser} = Z * \sin \theta$$

$$L_{ser} = X_{ser} / \omega$$

cancel reactance

$$Z = R_{ser}$$

$Z \neq R_s$ unless
design is right

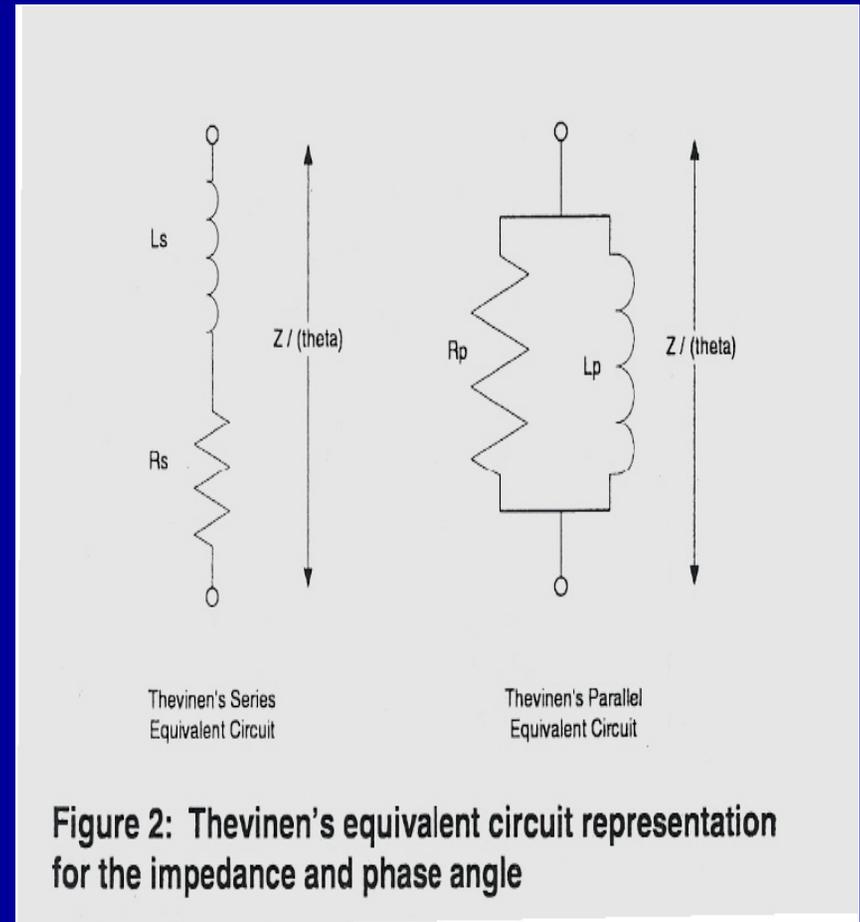


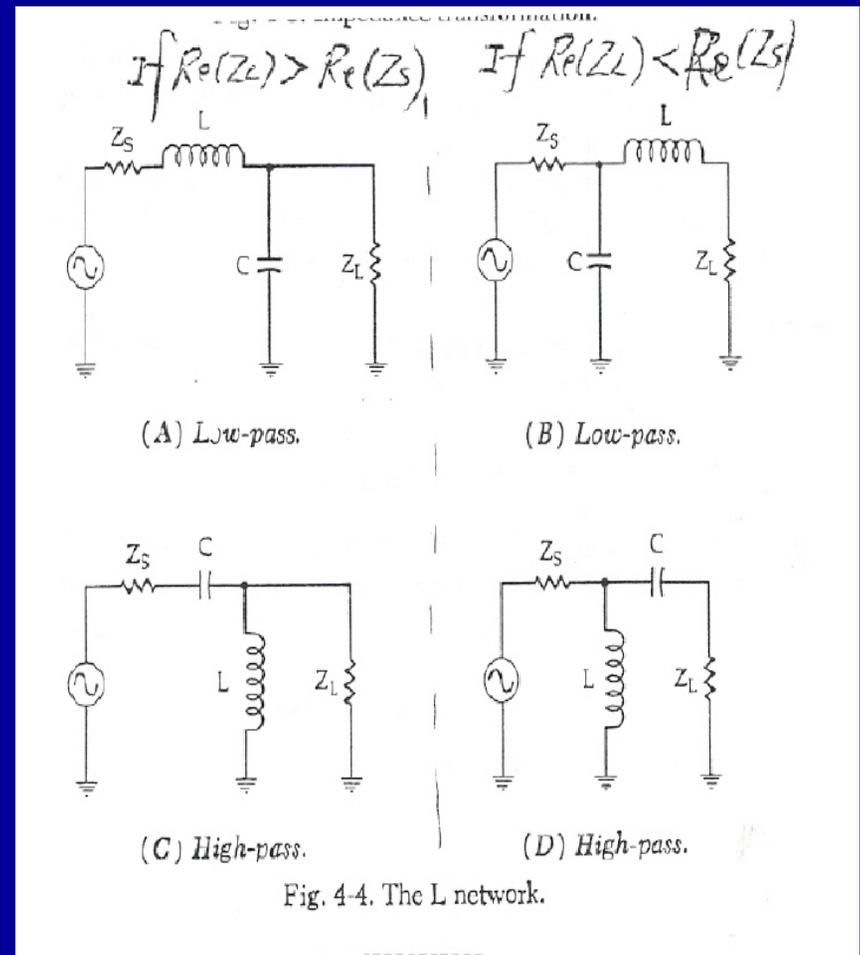
Figure 2: Thevenin's equivalent circuit representation for the impedance and phase angle

Tune Electrical Impedance

3. The L Network

Near lossless, max.
power transfer, esp.
if true conjugate of
 Z_s ; high or low pass
choose by:

$R_L > R_s, R_L < R_s$



Tune Electrical Impedance

3. L Network

High pass preferred for harmonic content, Nonlinear component increases rate of tissue necrosis due to increased absorption at focus (ref. 9);

components should be rated for power and values are at F,

technique can be written as a program

and can be extended to more complex T and π networks

can easily adjust for stray cap. and ind.

Tune Electrical Impedance

3. L Network

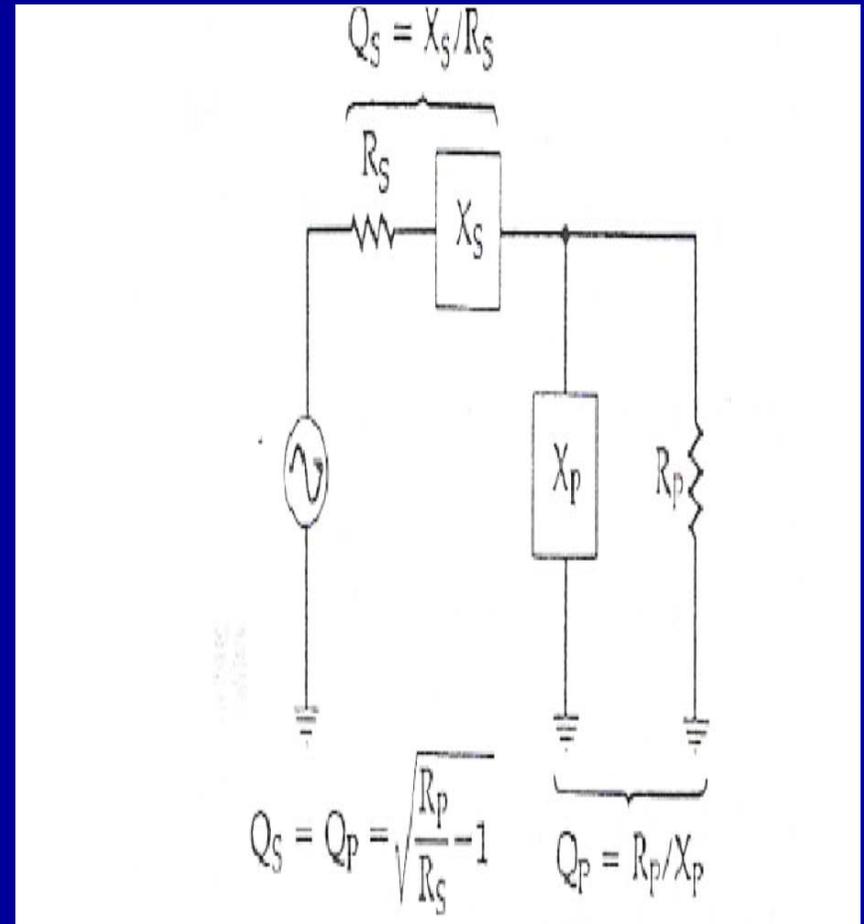
$$Q_s = Q_p = (R_p/R_s - 1)^{1/2}$$

$$X_s = Q_s * R_s$$

$$X_p = R_p / Q_p$$

$$L = X / \omega$$

$$C = 1 / (X * \omega)$$



Tune Electrical Impedance

Tuning Example

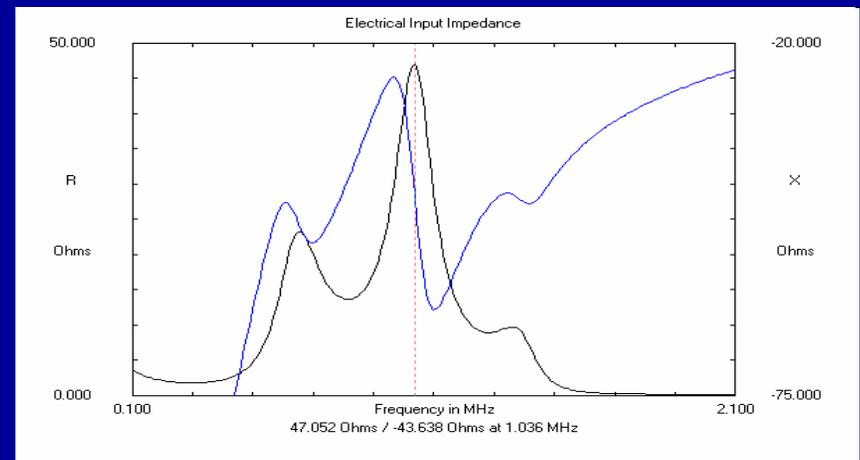
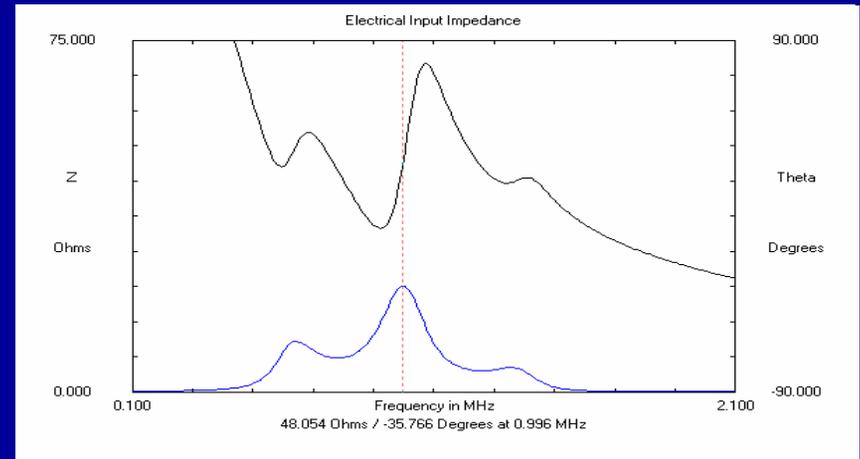
Double $\lambda/4$, Geo.
Mean

Use simple series L

$$L_s = X_s / \omega =$$

$$43.64 / 6.28 \times 10^6 =$$

$$6.95 \mu\text{H}$$

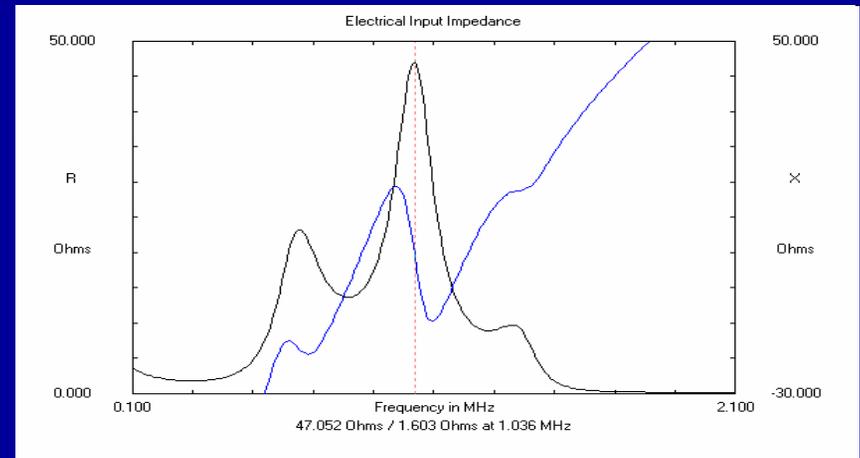
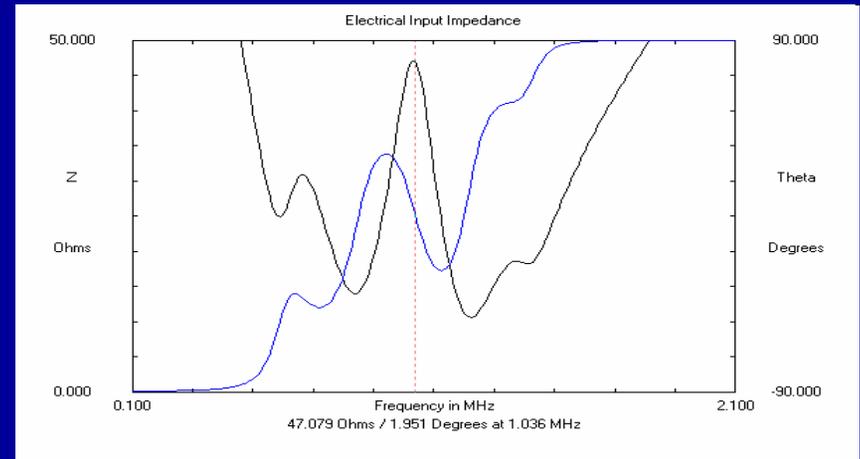


Tune Electrical Impedance

Results from
implementing into
model

$$Z \angle \theta = 47.1 \ \Omega \angle +2^\circ$$

$$R + jX = 47 + j 1.6$$

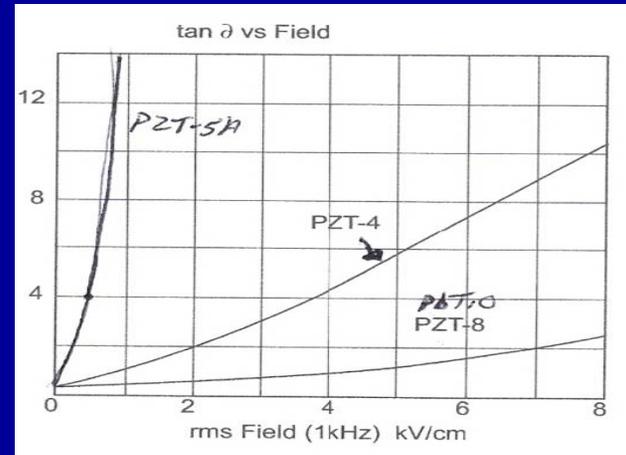
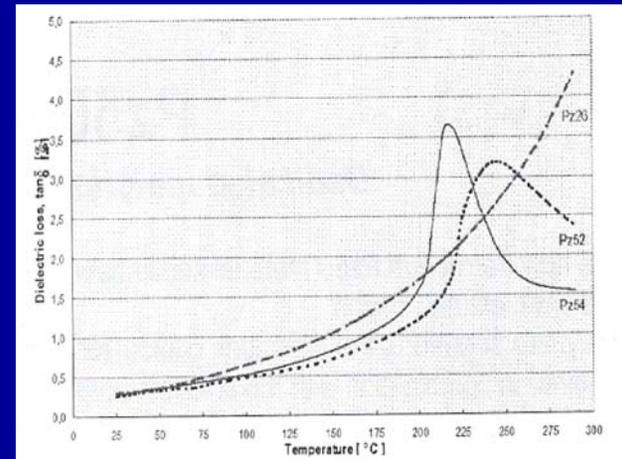


Consider Thermal Management

At high power, duty cycles – things will get hot!

To do:

1. Heat sink to thermal absorber
2. Thermal sensor
3. Coolant



Consider Thermal Management

Results:

Matching Layer and
electrode
delaminating,
blistering, cracking

Piezo cracking, depole
arcing, breakdown

Tuning Circuit and
Wires burnout



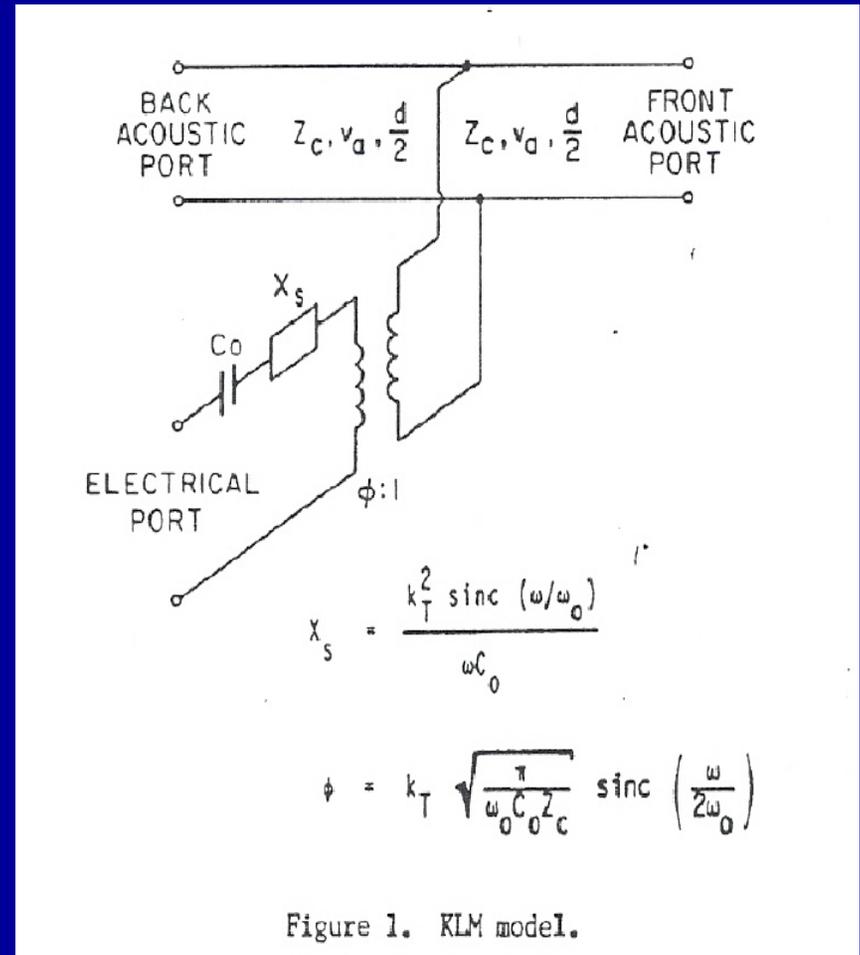
FIGURE 1. Cracked transducer front face due to an excessive applied power (about twice the maximal acceptable excitation level)

MODEL, MODEL, MODEL

1. Equivalent Circuits

- a. Mason's Model – Lumped element – not used except for simple devices
- b. Redwood – modified Mason's Model
- c. KLM – implemented in most software today
- d. Fs vs. Fp Operation

(ref. 1, 23 – 27)



MODEL, MODEL, MODEL

2. Implementation

a. Commercial SW Packages

1. PiezoCAD – 1-D , Sonic Concepts

2. ANSYS – FEA, Swanson

3. COMSOL – FEA,

4. PZFLEX – FEA, Weidlinger

b. Write own in C, MatLab, MatCad, Spice

MODEL, MODEL, MODEL

3. What can be done

- Predictive: Po, BW, IL, Imp, Field, Thermal**
- Parametric : include active & passive components, load losses**
- FEA: 2 & 3D, defects, mode coupling, etc**

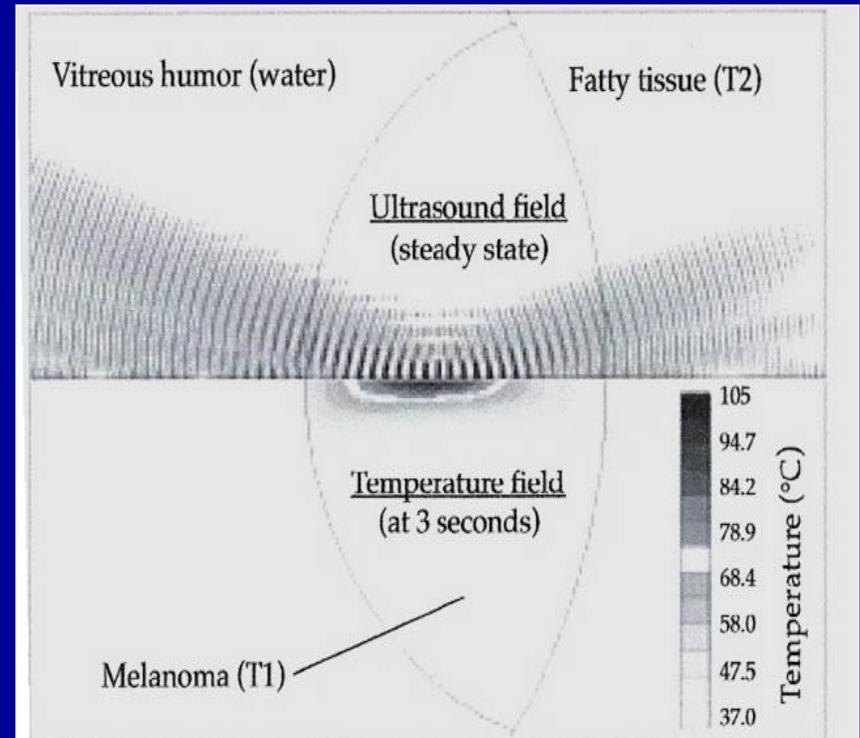


Figure 5. Axisymmetric model of an ocular tumor, showing focused ultrasound beam (above) and temperature distribution at 3 sec below). Note focal temperature in excess of 100 °C. The transducer as a 4 cm aperture and 9 cm focal length.

MODEL, MODEL, MODEL

4. An Example Using PiezoCAD

Single $\lambda/4$, $Z = 4.3$

No electrical tuning

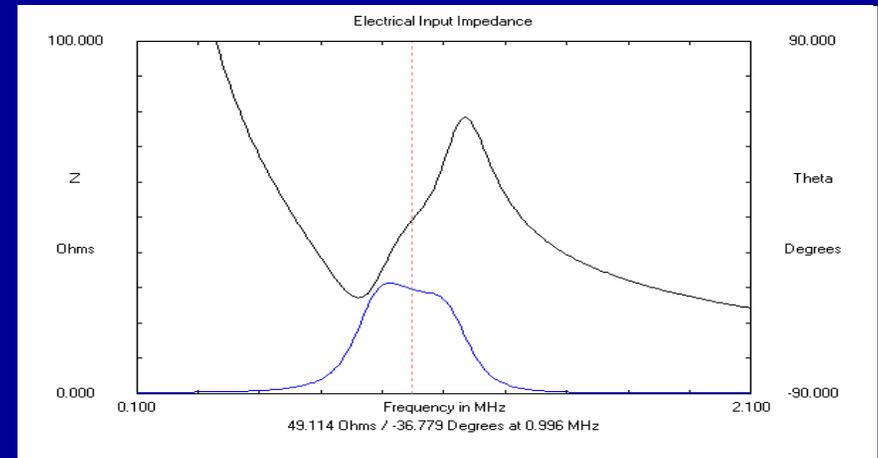
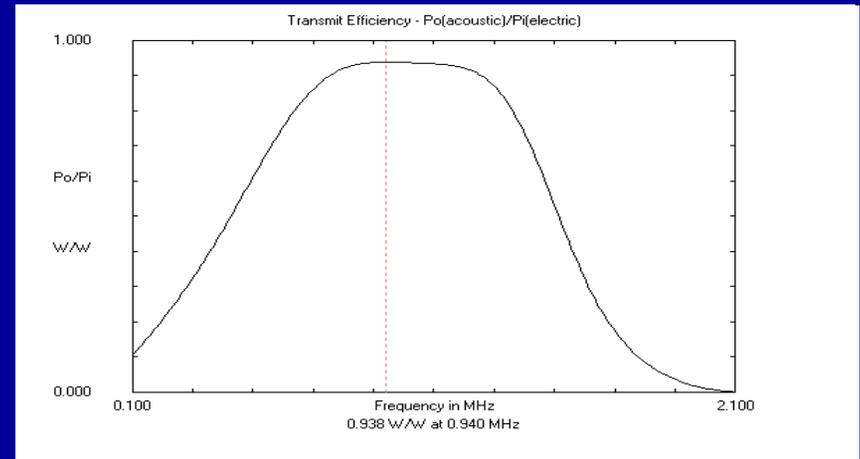
$Z / \theta = 49 / -37 @ 1M$

$P_o/P_i = .938 W/W @ .94$

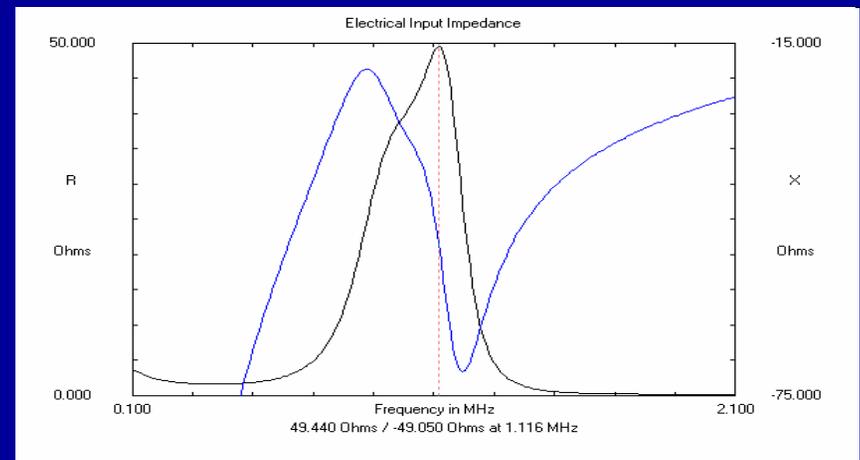
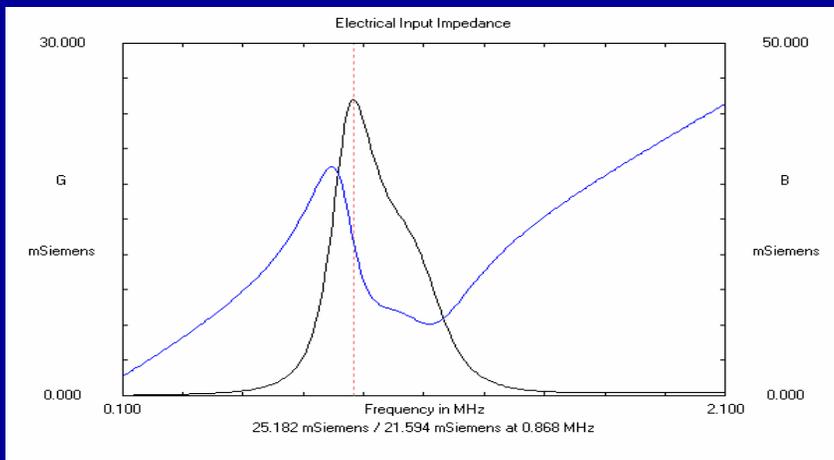
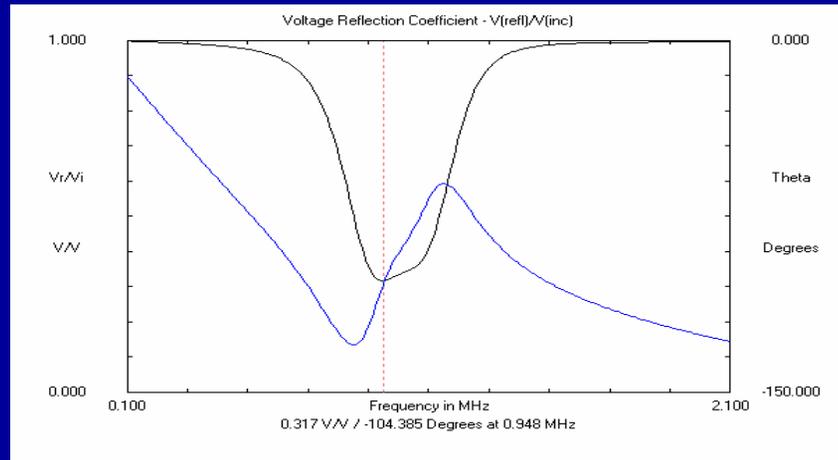
$R_{max} = 49 @ 1.116 M$

$G_p @ .868 M$

$VRC = .317 V/V @ .95 M$



MODEL, MODEL, MODEL



MODEL, MODEL, MODEL

Adjust Matching Layer
Thickness to affect F, R

$$P_o/P_i = .944 \text{ W/W @ } .97$$

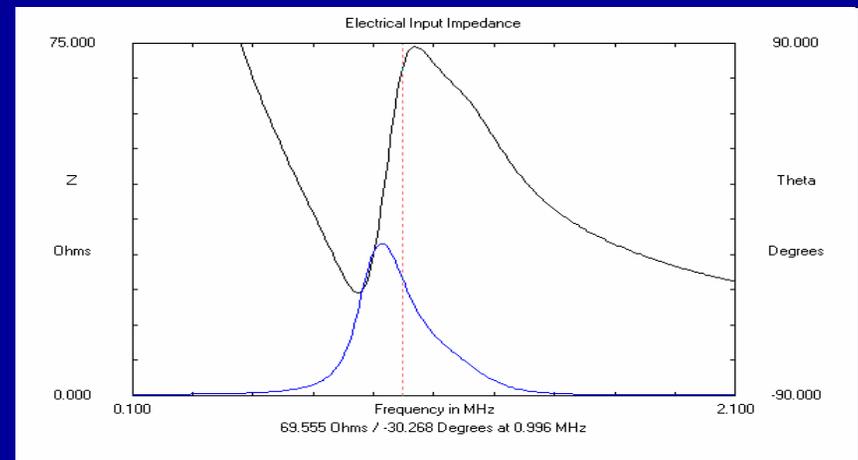
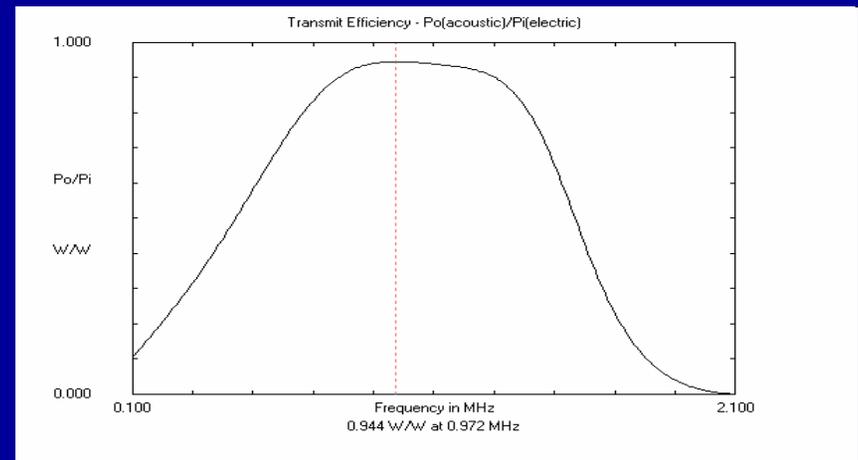
$$Z / \theta = 69.5 / -30 \text{ @ } 1 \text{ M}$$

$$G_p \text{ @ } .876 \text{ M}$$

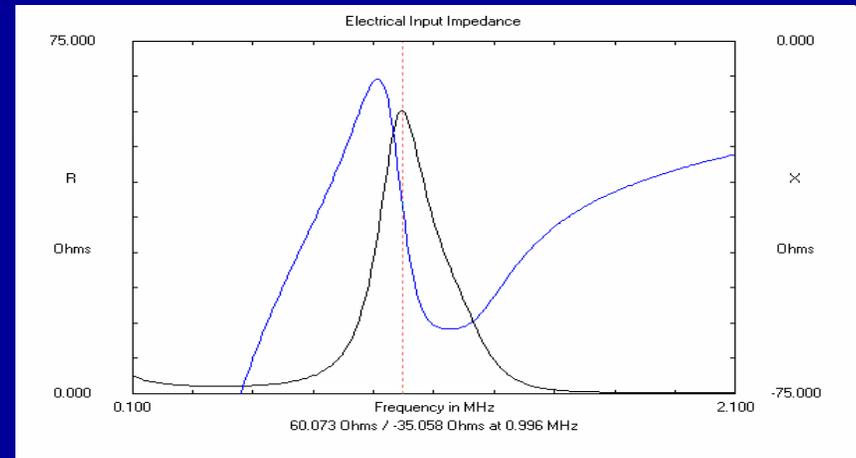
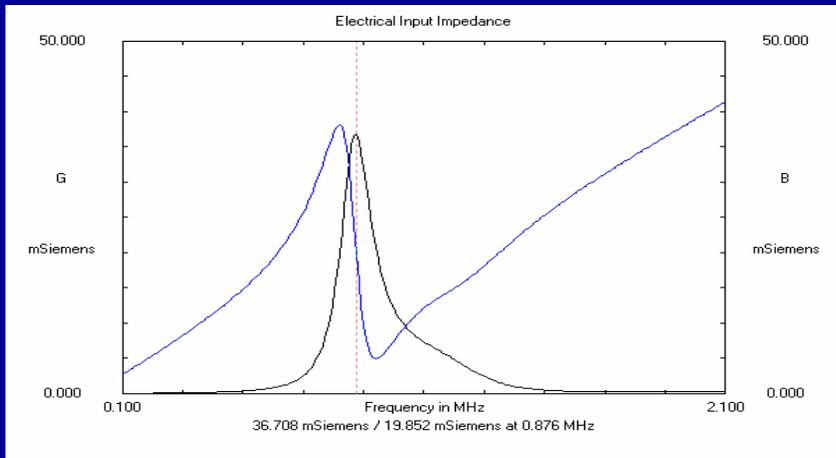
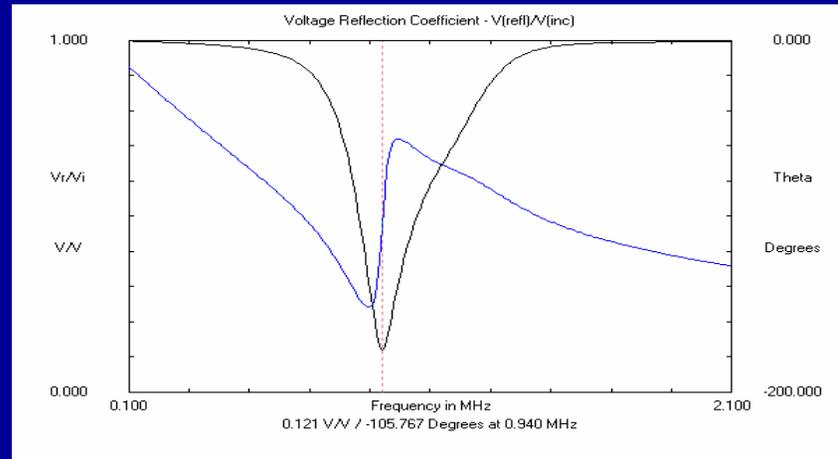
AND

$$R_{\text{max}} = 60 \text{ @ } 1 \text{ M}$$

$$\text{VRC} = .121 \text{ V/V @ } .94$$



MODEL, MODEL, MODEL



MODEL, MODEL, MODEL

Add Tuning to cancel reactance
Series L = 5.6 μH @ 1 M

Results

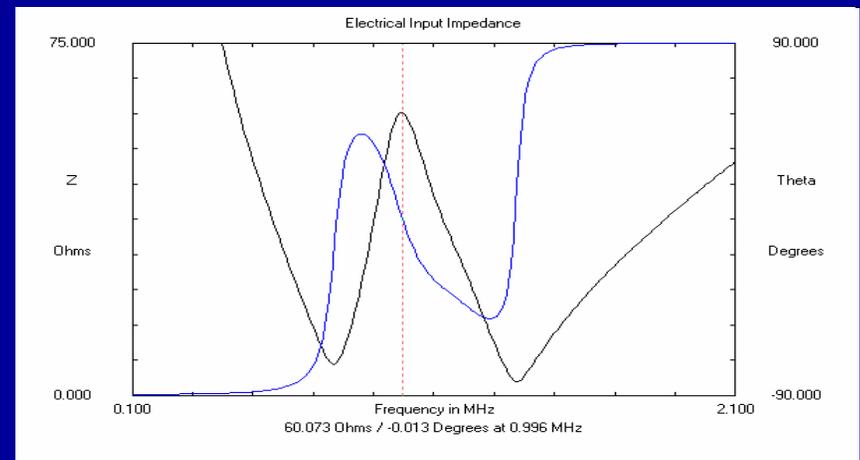
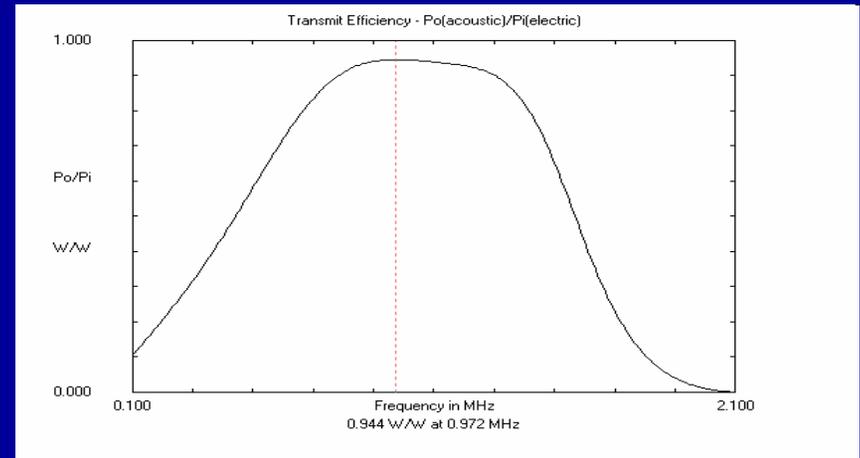
$P_o/P_i = .944 \text{ W/W} @ .97$

$Z / \theta = 60 / 0 @ 1 \text{ M}$

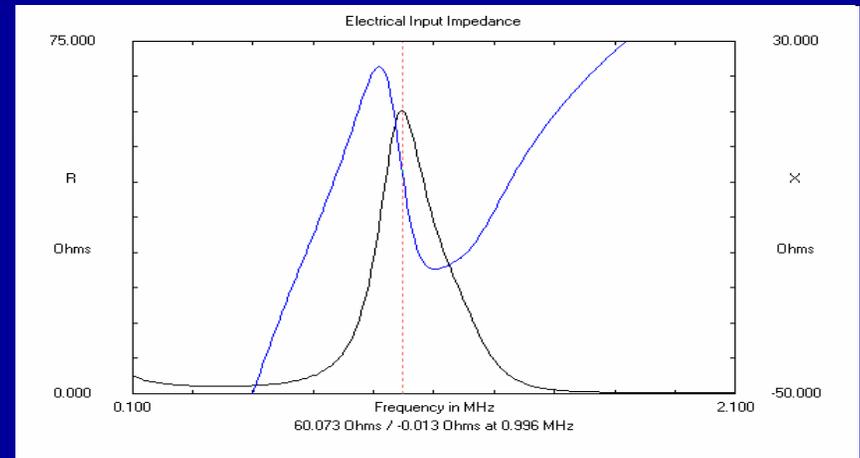
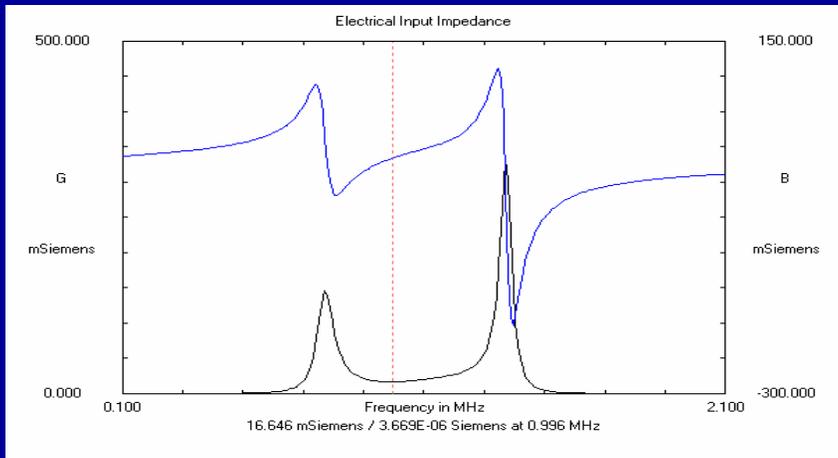
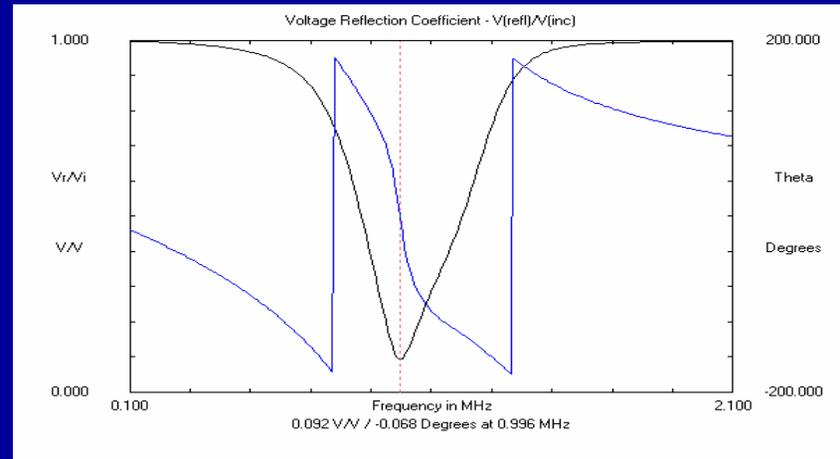
R max = 60 @ 1 M

VRC = .09 V/V @ 1 M

G shows typical split peaks



MODEL, MODEL, MODEL



Consider MRI Compatibility

1. Material Selection

- a. **Compatible:** polymers, carbon & graphite, copper, brass, BeCu, glasses & ceramics: fused silica, quartz, Macor, ZrO, AlO, AlN, SiN, Wood
- b. **Safe:** Aluminum, Titanium, Gold, Platinum, Palladium, Silver, some Stainless Steels, most piezo materials – some contain iron, nickel, gadolinium – be sure of trace additives
- c. **Dangerous:** magnetic / para-magnetic materials – iron and compounds, nickel, gadolinium, some piezo's

(ref's: 28,29)

Consider MRI Compatibility

2. Design Issues

- a. long cable runs from source, typ 7 to 10 M, signal losses
- b. can not electrically tune @ the transducer with coils, chokes, transformers
- c. avoid internal wire loops – can cause stray inductances
- d. exercise caution with fillers in polymers – know purity

Consider MRI Compatibility

3. Verification of Product

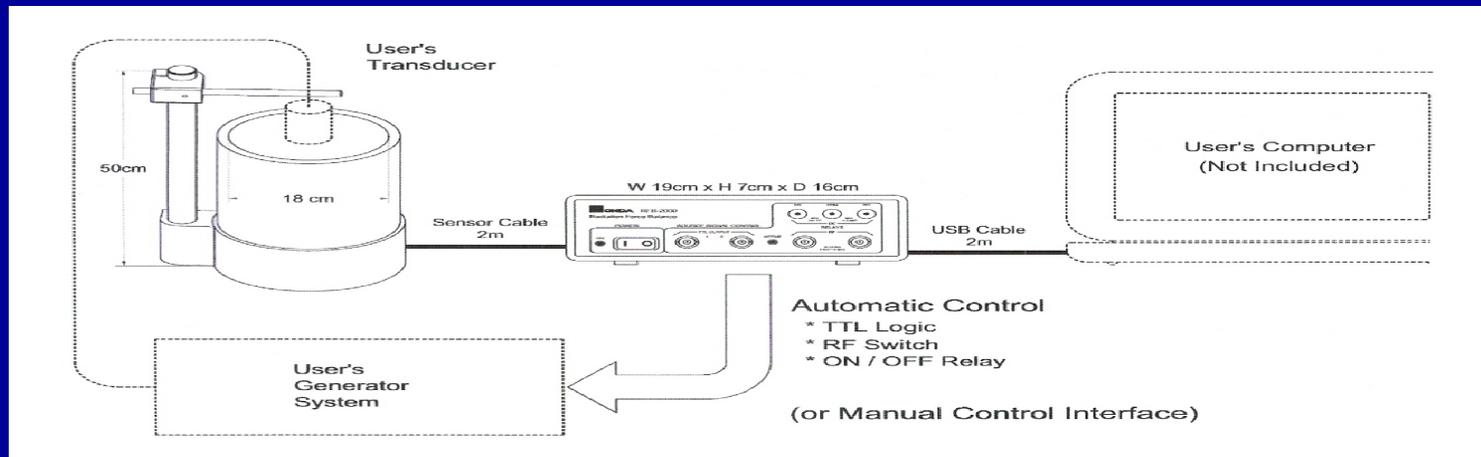
ASTM, ANSI, ISO, IEC, NEC, FDA and others all publish standards for Testing Methods, Labeling Requirements, Definitions, etc.

www.mrisafety.org

Test and Characterize Performance, Life and Safety

ref (4, 30 – 35, 57)

1. Attended the preceding workshop “Acoustic Output Measurements”, Mark Hodnett, NPL
2. Standards Bodies: IEC, FDA, AIUM, ANSI, NEC, NEMA, etc.
3. Testing – parameters, output, linearity, repeatability, life expectancy, safety
 - a. Output Power – TAP Meter, RF Amp, FG, PC, O’scope



Test and Characterize Performance, Life and Safety

3. Testing

b. Sound Field

- 1. Scanning Tank with Hydrophone: 5 – 6 axis of freedom, can map in 3D, low power BUT new high power hydrophones being developed**

Test and Characterize Performance, Life and Safety

3. Testing

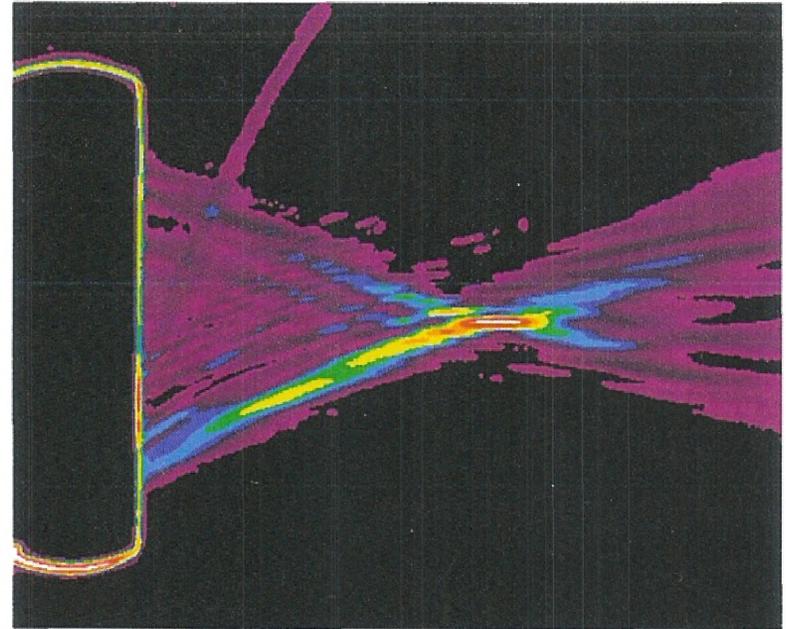
b. Sound Field

2. Schlieren Optical

High resolution,

can identify flaws or non-uniformities at low & high power,
power,

Software can do 3D



Highly focused beam showing anomalous sidelobe caused by a crack in the radiating surface.

Test and Characterize Performance, Life and Safety

3. Testing

b. Sound Field

3. Acoustic Streaming (57)

similar to Schlieren but uses suspended particles to map velocity profiles

4. Phantoms

several sources for HIFU phantoms, reasonably clear and closely mimic tissue, can visualize treatment

Test and Characterize Performance, Life and Safety

3. Testing

c. Environmental

1. Thermal Conditions: storage, shipping, operating
2. Hermiticity: IP rating, splash, immersion, etc., gas sterilization
3. ESS/ Burn-in: validate to full spec
4. Accelerated Life
5. FMEA

d. Electrical Safety

1. HiPot
2. Insulation Resistance
3. Current Leakage
4. EMI/ EMS

Test and Characterize Performance, Life and Safety

4. Safety

- a. use common sense
- b. always operate loaded
- c. Always make sure source is off when connecting or disconnecting
- d. always use degassed water
- e. know limits
- f. always have path to ground
- g. **NO BODY PARTS!**



FIGURE 1. Cracked transducer front face due to an excessive applied power (about twice the maximal acceptable excitation level)

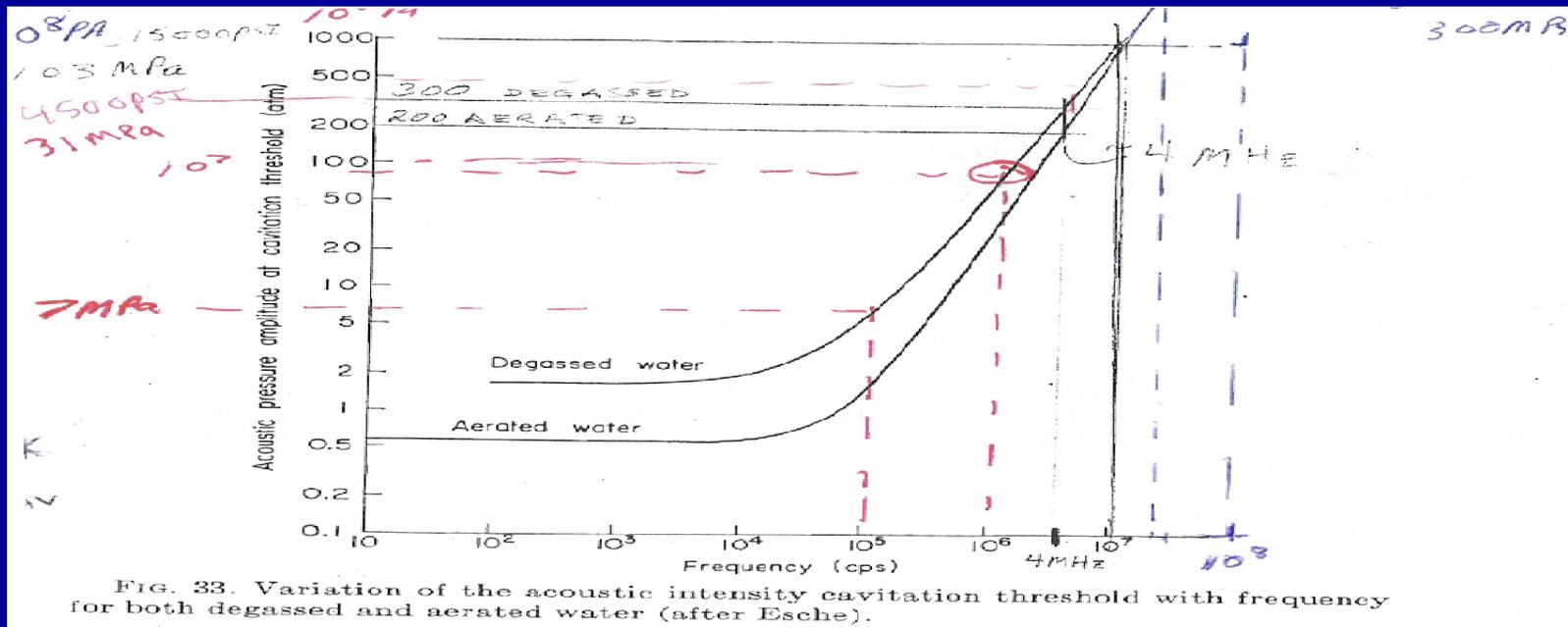
Consider Other Uses

ref (38 – 41)

1. Industrial

- a. Droplet Jetting: basically same as HIFU , must know material properties; ex. Ink jets, coating
- b. Nebulize / Atomize: chemical analyzers, FUSION

$$d = .34 * (\pi^3 * T / (\rho * F^2))^{1/3}$$



Consider Other Uses

1. Industrial

c. Megasonic Cleaning – uses streaming

d. Descaling – think Lithotripsy

e. Pumps – streaming

2. Pharma / Consumer

a. Cosmetic – skin / wrinkle enhancement

b. nebulizers – inhalable drugs – asthma, diabetes

c. needleless injection – drugs that are too large

References

1. “Efficiency of Excitation of Piezoceramic Transducers at Antiresonance Frequency”, A.V. Mezheritsky, Transactions on Ultrasonics, Ferroelectrics and Frequency Control (UFFC), Vol 49, No. 4, April 2002
2. Guide to Modern Piezoelectric Ceramics, Morgan Electroceramics, can download from website
3. “The Design of Efficient Broadband Piezoelectric Transducers”, Charles S. DeSilets et al, Transactions on UFFC, Vol. SU 25, No. 3, May 1978
4. Material Properties PDF download, ONDA Corp. (www.ondacorp.com)
5. “Impedance Matching for Maximizing Transducer Performance”, Ron McKeighen, PSU NIH Transducer Resource Center Newsletter 2001
6. “Impedance Matching”, RF Circuit Design
7. “Broadband Transformers and Power Combining Techniques for RF”, H. Granberg, Motorola RF Device Data AN749
8. “Notes on the Design of Matching Systems for Piezoelements” AirMAr Technology Corp. Application Notes, 1997
9. Therapeutic Ultrasound Tutorial, Dr. Lawrence Crum, IEEE Ultrasonics Symposium, NY,NY, Oct., 2007
10. “Guiding HIFU Therapy in Real Time using Cavitation Noise Diagnostics”, R. A. Roy, et al, IEEE US Symp., NY, NY, Oct. 2007
11. “Efficient Array Design for Sonotherapy Enhanced Drug Delivery”, D. Stephens, et al, IEEE US Symp., NY, NY, Oct. 2007
12. “Interactions of High Intensity Focused Ultrasound with Biological Materials”, Ajit Mal, et al, SPIE NDE & Smart Structures Symposium, San Diego, CA, March 2002

References

13. "The Use of Broadband Signals to Reduce Grating Lobe Effects in HIFU Tissue Ablation", F. Dupenloup, et al, Proceedings of the IEEE US Symp. 1994
14. "Mid to High Power Imaging Arrays from ARFI to HIFU", M. J. Zipparo, Proceedings of the IEEE US Symp. 2003
15. "Beamforming for Therapy with High Intensity Focused Ultrasound (HIFU) using Quantitative...", C. I. Zanelli, et al, Proceedings of the IEEE US Symp. 1993
16. "A Transvaginal Image-Guided High Intensity Ultrasound Array", S. Vaezy, et al, Proceedings of the IEEE US Symp. 2003
17. "Effect of Matching Layer on Acoustic Lens on Suppressing Lamb Wave Formation", J. Kubota, et al, Proceedings of the IEEE US Symp. 2003
18. "Development of small High Intensity Focused Transducers for Ultrasound Endotherapy", J. Y. Chapelon, et al, Proceedings of the IEEE US Symp. 1996
19. "A Laparoscopic HIFU Probe for Kidney Ablation prior to a Partial Nephrectomy", Jahangir Tavakkoli, et al, Proceedings of the IEEE US Symp. 2001
20. "Self-Focusing HIFU Source for Large Therapy Volumes", J. Hoffelner, et al, Proceedings of the IEEE US Symp. 1998
21. "Design and Characterization of a 10 cm Annular Array Transducer for High Intensity Focused Ultrasound (HIFU) Applications", C. I. Zanelli, et al, Proceedings of the IEEE US Symp. 1994
22. "Designing a HIFU Transducer to Stop Gastrointestinal Bleeding", Poster on U of WA website: www.waspacegrant.org/graphics/posters/HIFtransducer.jpg
23. "Comparison of the Mason & KLM Equivalent Circuits for Piezoelectric Resonators in the Thickness Mode", Stewart Sherrit, et al, Proceedings of the IEEE US Symp. 1999

References

24. "Equivalent Circuits for Transducers having Arbitrary Even – or – Odd Symmetry Piezoelectric Excitation", David A. Leedom, et al, IEEE Transactions on Sonics and Ultrasonics, Vol. Su-18, No. 3, July 1971
25. "KLM Model Implementation using Transfer Matrices", Alan R. Selfridge, Ultrasonic Devices Inc., S. Gelbach, Kesa Corp.
26. "The Value of Models in Transducer Design", Clyde G. Oakley, M. Zipparo, Tetrad (Gore) Corp., PSU NIH Transducer Resource Center Ultrasound Transducer Engineering Conference, Aug. 2000
27. "Nonlinear Modeling of Therapeutic Ultrasound", G. Wojcik, et al, Proceedings of the IEEE US Symp. 1995
28. "Integrating Ultrasound Transducer with MRI for Therapeutic and Diagnostic Applications", Rajiv Chopra, IEEE US Symp., NY, NY, Oct 2007
29. "MRI Detection of Increased Bloodflow due to Low Amplitude Pulsed Ultrasound Stimulus", J. Brosch, G. A. Morris, Piezotech, LLC, IEEE US Symp. Poster 2001
30. "Development of a High Intensity Focused Ultrasound (HIFU) Hydrophone System", Mark Schafer, et al, Proceedings of the IEEE US Symp. 2005
31. "High Intensity Focused Ultrasound Calibration – Status and Challenges", I. H. Rivens, G. R. terHaar, 2004 Journal of Physics Conference Series 1
32. "Safety Issues for HIFU Transducer Design" G. Fleury, et al, pdf download Imasonic website, www.imasonic.com
33. "Development and Characterization of an Innovative Synthetic Tissue – mimicking Material...", Cyril Lafon, et al, Proceedings of the IEEE US Symp. 2001
34. "High Resolution Mapping og Nonlinear MHz Ultrasonic Fields using a Scanned Scatterer", P. Kaezkowski, et al, Proceedings of the IEEE US Symp. 2003

References

35. **“Characterization of High Intensity Focused Ultrasound Fields...” M. S. Canney, Proceedings of the IEEE US Symp. 2006**
36. **“NewPiezocomposite Transducers for Therapeutic Ultrasound”, G. Fleury, et al, International Society for Therapeutic Ultrasound Symposium 2002; can download from Imasonic website**
37. **“High Intensity Ultrasound Focusing by Optimal Design of an Acoustic Lens”, no author listed, found on web search keyword “HIFU”**
38. **“Effect of Liquid Properties on the Production of Aerosols with Ultrasound”, J. Sears, et al, Proceedings of the IEEE US Symp. 1977**
39. **“Evaluation and Design of New Piezoelectric Droplets Generator”, A. Giovannini, et al, Proceedings of the IEEE US Symp. 1994**
40. **“Ultrasound Controlled Taylor-Mode Breakup of Liquid Jets”, S. C. Tsai, et al, Proceedings of the IEEE US Symp. 1997**
41. **“High Power Density Prototype for High Precision Transcranial Therapy”, M. Pernot, et al, pdf download from Imasonic website**
42. **“Design and Development of a Prototype Endocavitary Probe for High Intensity Focused Ultrasound Delivery with Integrated MRI”, Iain P. Wharton, et al, Journal of MRI, Vol. 25, issue 3, Feb. 2007**
43. **“Distance Size Dependency of Necrotic Region of Variable Focal Length HIFU Transducerwith Lens and Linear Array”, K. Ishida, et al, Proceedings of the IEEE US Symp. 2002**
44. **“Development of a High Intensity Focused Ultrasound System for Image-guided Ultrasound Surgery”, Peter J. Kaczowski, et al, 142nd Meeting of the Acoustical Society of America**
45. **“Toric HIFU Transducer for Large Thermal Ablation”, David Melodlima, et al, Proceedings of the IEEE EM&BS Conference 2007**

References

46. US Patent 5492126, "Probe for Medical Imaging & Theray using Ultrasound", C. Hennige, E. Driscoll, assigned to Focus Surgery Inc.
47. US Patent 6716184, "Ultrasound Therapy Head Configured to Couple to an Ultrasound Imaging Probe..." \, Roy W. Martin, et al, assigned to University of Washington
48. "Usinf Sound to See and Stop Bleeds", Neil Owen, et al, 146th Meeting of the Acoustical Society of America, 2003
49. "A HIFU System using Annular and Strip Electrode Arrays....", R. Muratore, Proceedings of the IEEE US Symp. 2004
50. "Comparison of Split-Beam Transducer Configuration Geometry and Excitation Configurations...", Ralf Seip, et al, Proceedings of the IEEE US Symp. 2001
51. "Firing Session Optimization for Dynamic Focusing HIFU Treatment", L. Curiel, et al, Proceedings of the IEEE US Symp. 2000
52. "InSitu Thermal Parameter Estimation for HIFU Therapy Planning and Treatment Monitoring", A. Anand, et al, Proceedings of the IEEE US Symp. 2004
53. "A Phased Array Antenna for Simultaneous HIFU Therapy and Sonography", T. Sheljaskov, et al, Proceedings of the IEEE US Symp. 1996
54. "On-line Assessment of HIFU Beams and Lesion Monitoring using Dual-Transducer Modes", F. L. Lizzi et al, Proceedings of the IEEE US Symp. 2003
55. "A Polyacrylamide Gel Acoustic Coupling Medium for Therapy Applications....", A. Prokop, et al, Proceedings of the IEEE US Symp. 2001
56. "Effect of Beam Asymmetryon Ultrasound Thermal Lesions", F. L. Lizzi, et al, Proceedings of the IEEE US symp. 1999
57. "Chacterization of High Intensity Focused Ultrasound Transducers using Acoustic Streaming", Prasanna Hariharan, et al, Journal of the Acoustic Society of America, Vol. 123, No. 3, March 2008, pp 1706 – 1719